

# Physics & Technology of Multi-slice CT

James Weston

ImPACT

- Some key factors about MSCT
  - construction of scanners
  - reconstruction techniques
  - artefacts
  - other factors
- Concepts and ideas
  - keep it non-mathematical!

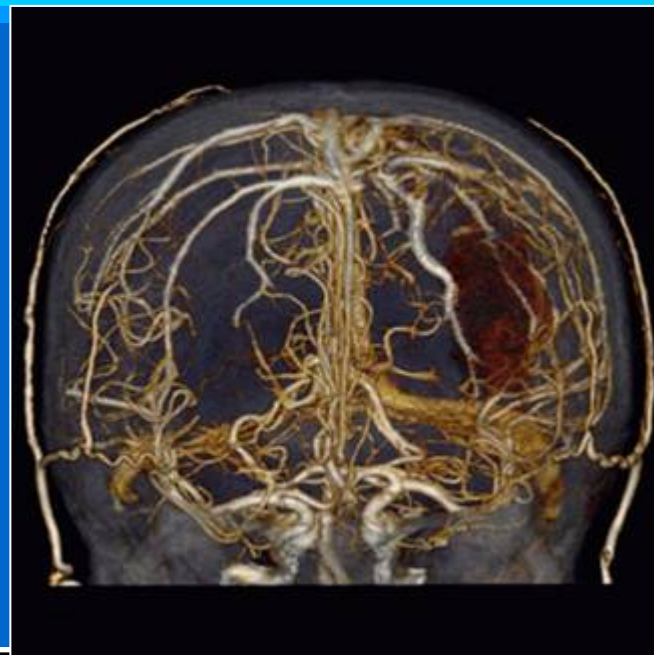
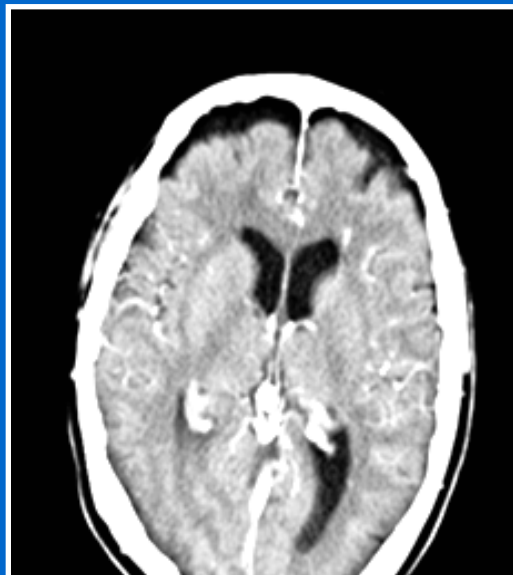
# MSCT scanners

- 1991 Dual slice
- 1998 Four slice
- 2002 16 slice
- 2003 32 slice
- today
  - 64 sub-mm slices
  - 0.4 s rotation



# Clinical scanners

- Image quality and capability increasing



# The 3 Fs of CT

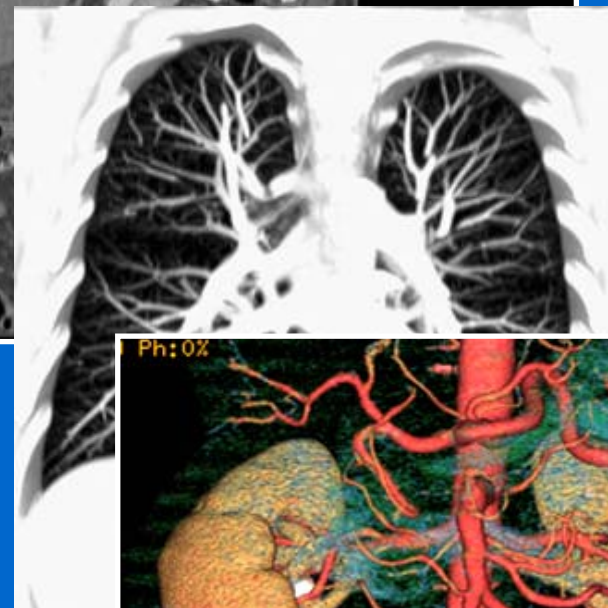
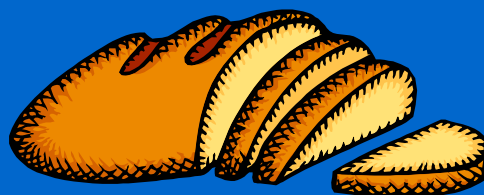
- **Faster**



- **Further**



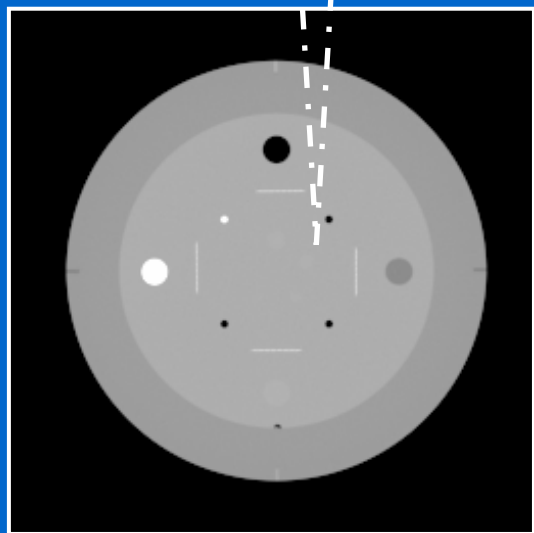
- **Finer**



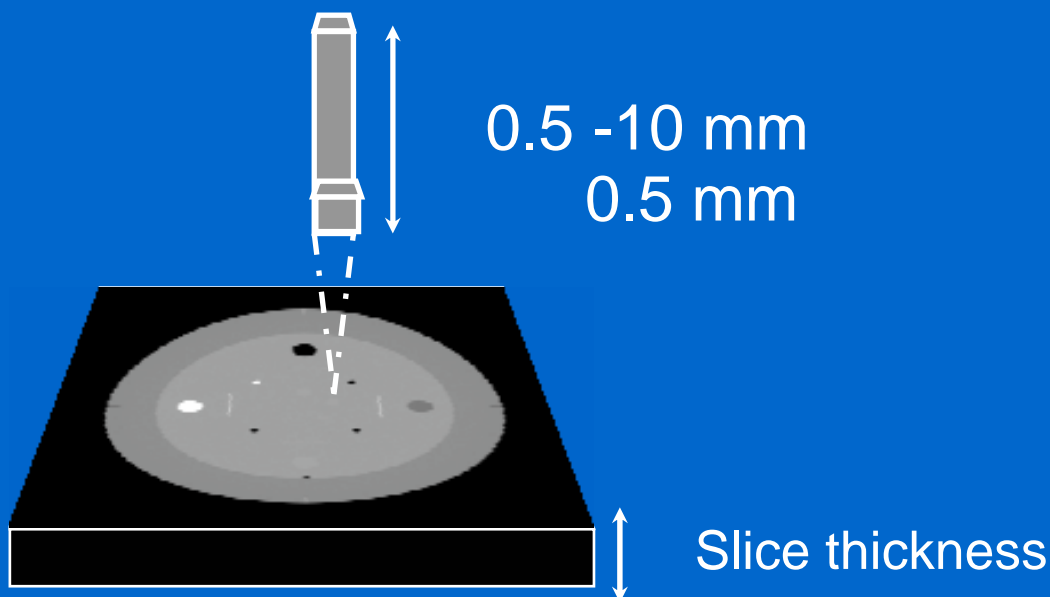
# Isotropic imaging

- 2D pixel in a CT image represents a 3D voxel
- Resolution is ideal when equal in all 3 dimensions
  - best results with slice thickness equal to (axial) pixel size
  - routine 0.5 - 1 mm slice thickness achieves this goal

0.5 x 0.5 mm

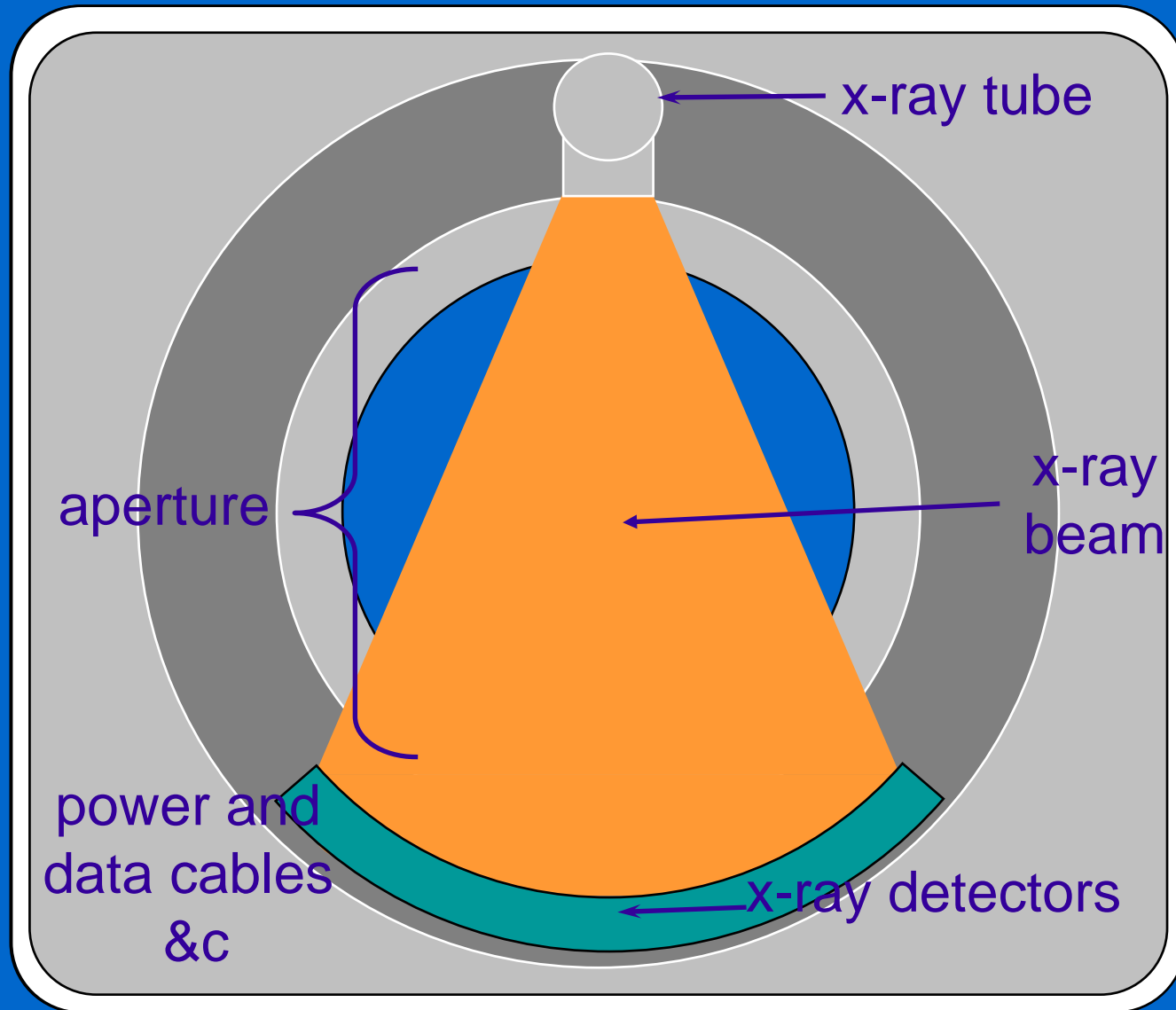


0.5 - 10 mm  
0.5 mm



# Scanner design

- What's under the covers ?

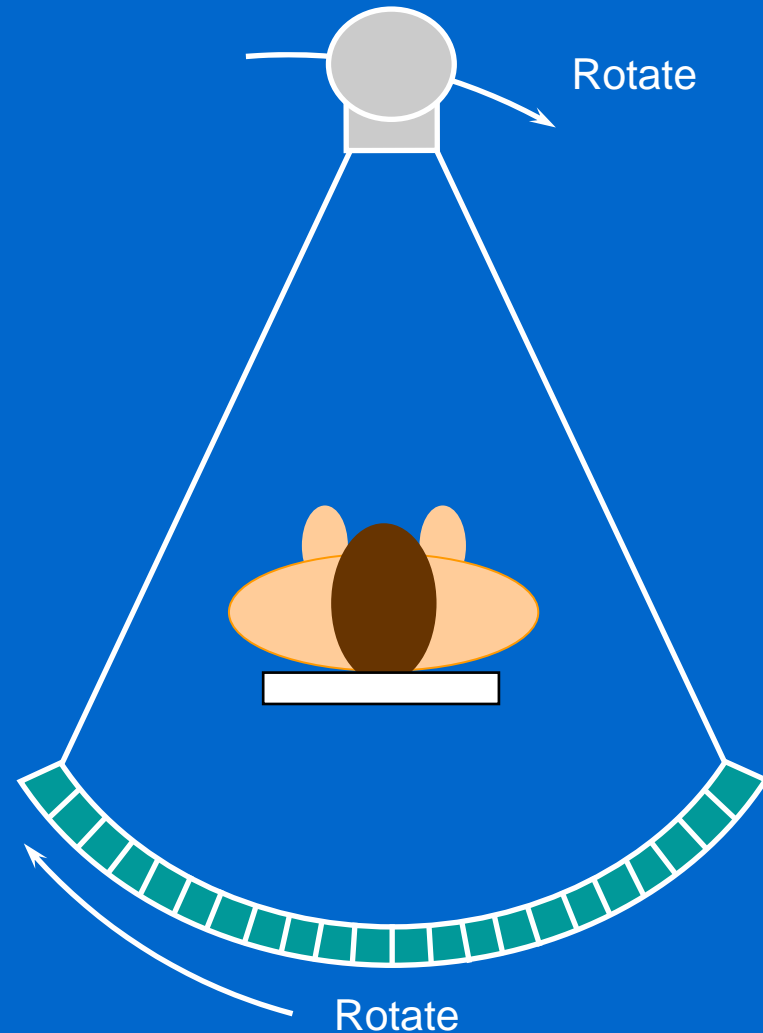


# “Third generation” CT scanners

- Tube & detectors
  - rotate around patient gathering x-ray projections
- Projection data used to form slice images
  - filtered back projection



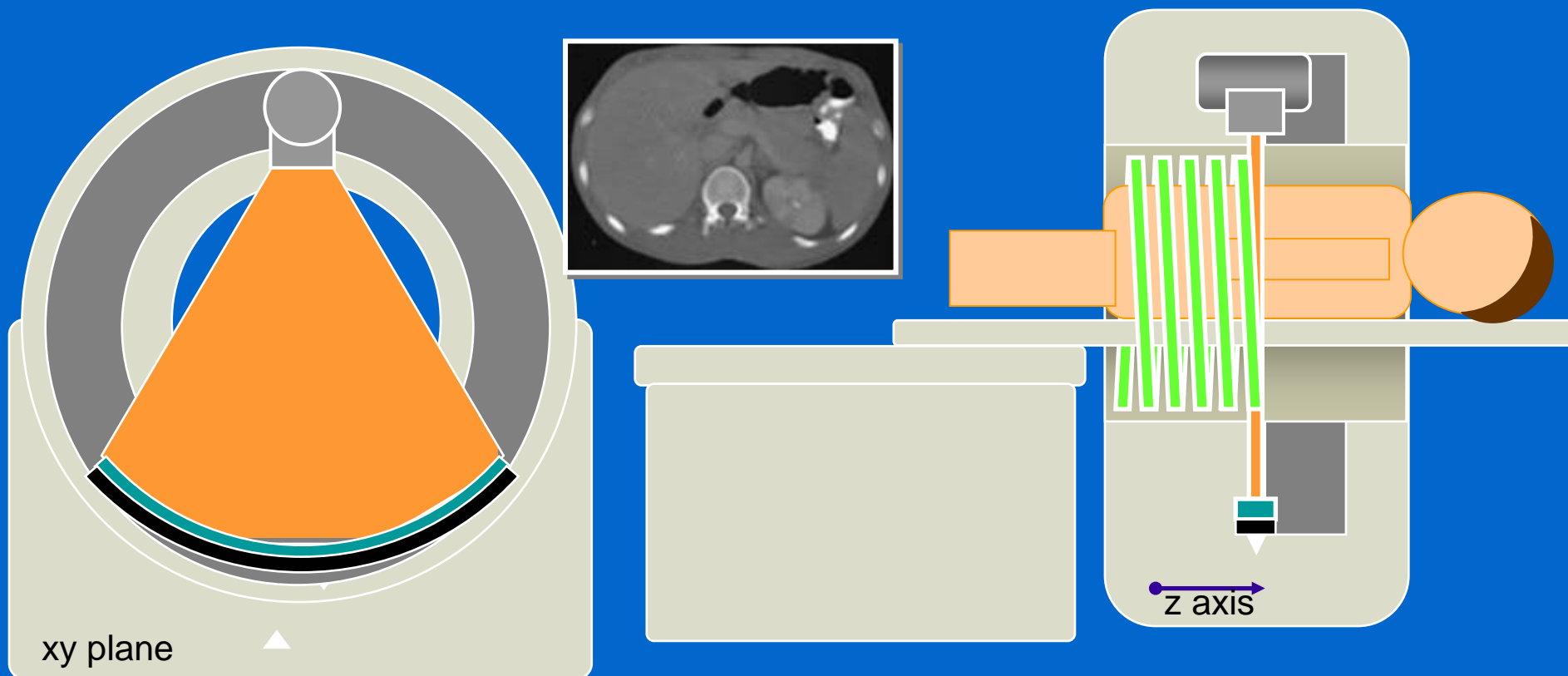
Rotate – Rotate  
the modern scanner design





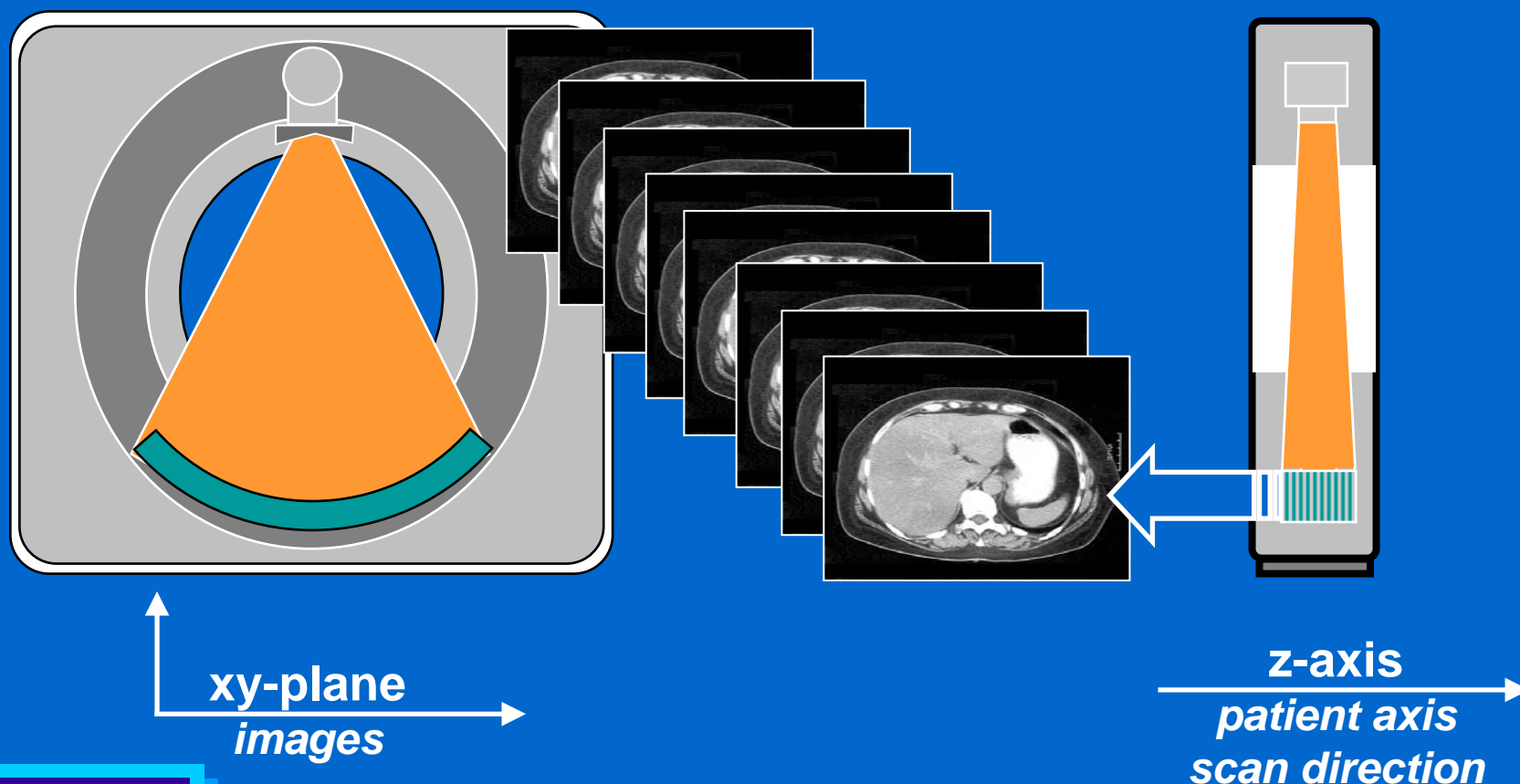
# Helical CT

- Continuous gantry rotation + continuous table feed
- Scan data traces a helical path - or 'spiral' - around patient
  - data used to form axial images

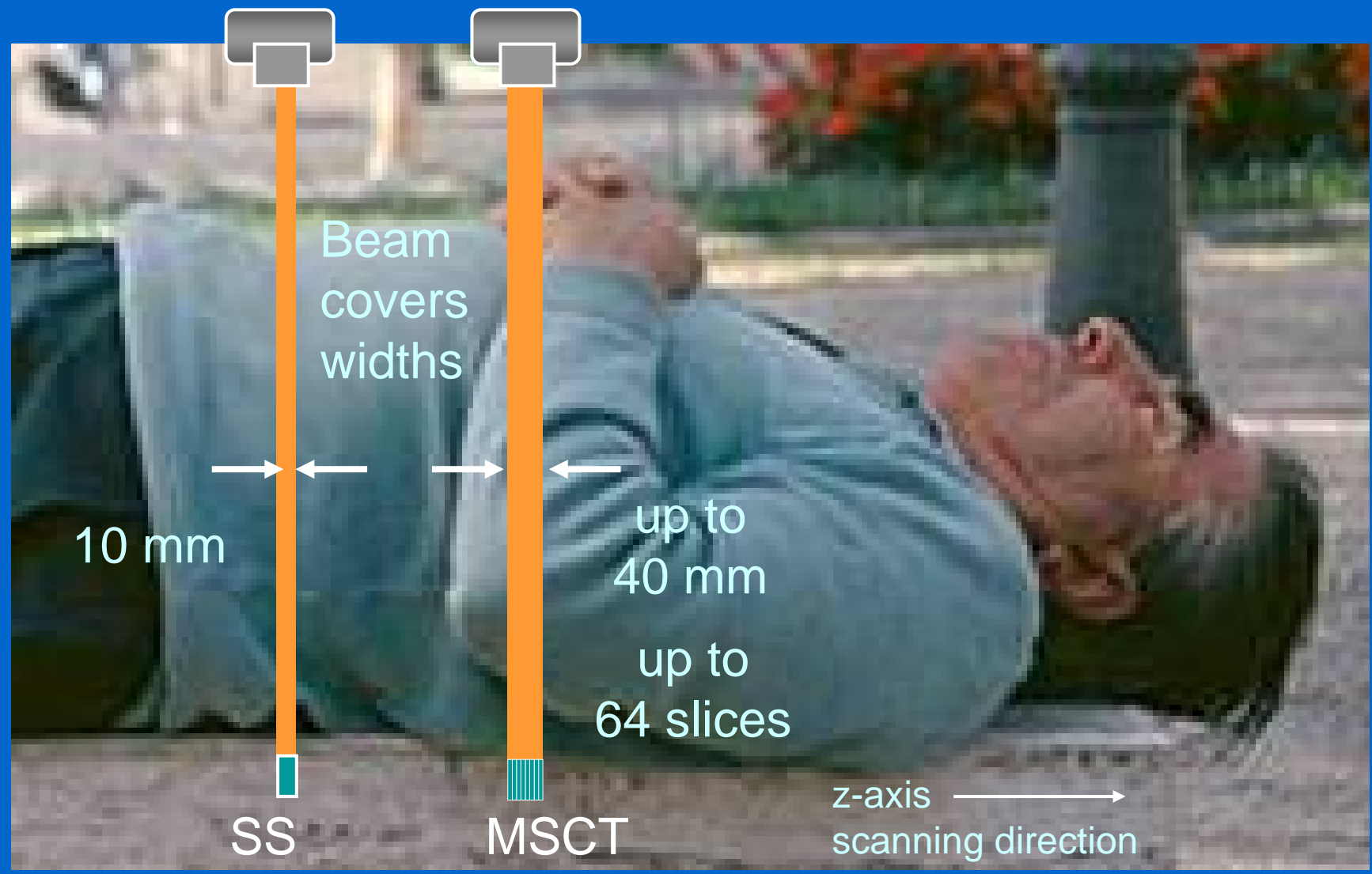


# Multi-slice CT scanning

- Many features in common with single slice (SSCT)
  - multiple parallel detector banks along z-axis
  - enables a number of projections to be acquired simultaneously

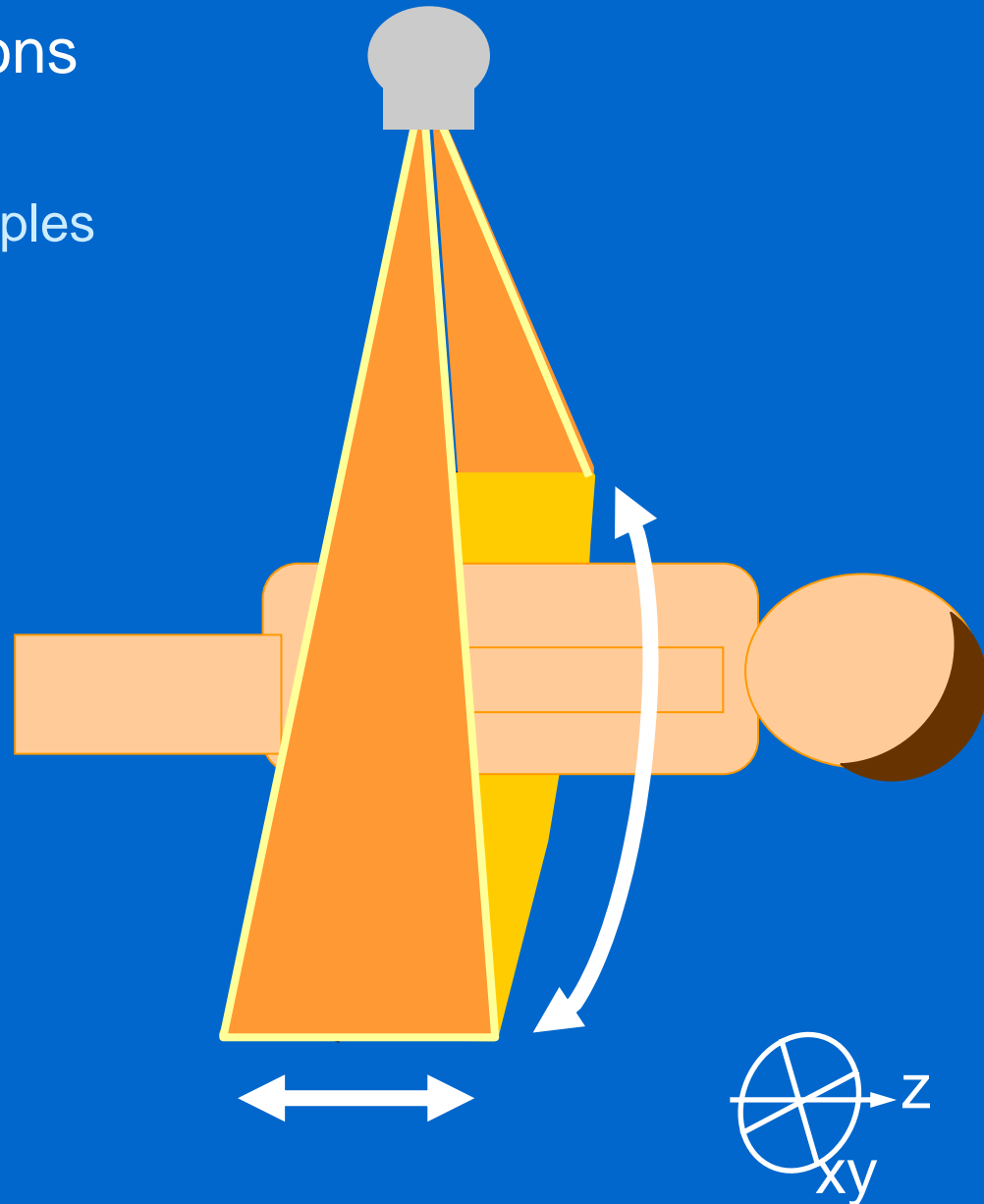


# MSCT scanning: in scale



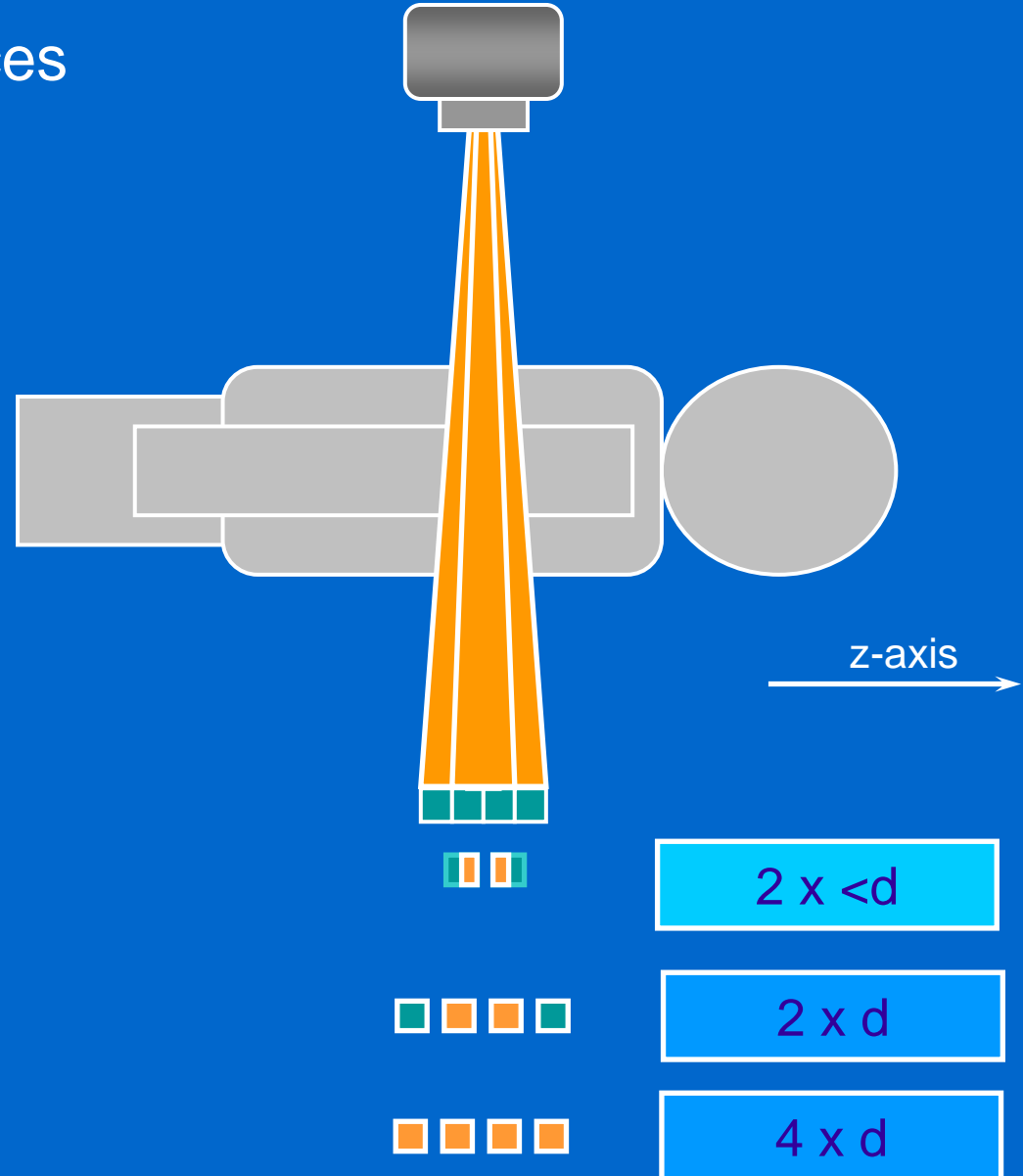
# Detector banks

- Array extends in 2 directions
  - xy-plane
    - arc to collect many samples for each projection
  - z-axis
    - along the patient length
- SSCT
  - z-axis coverage: one element
- MSCT
  - many z-axis elements



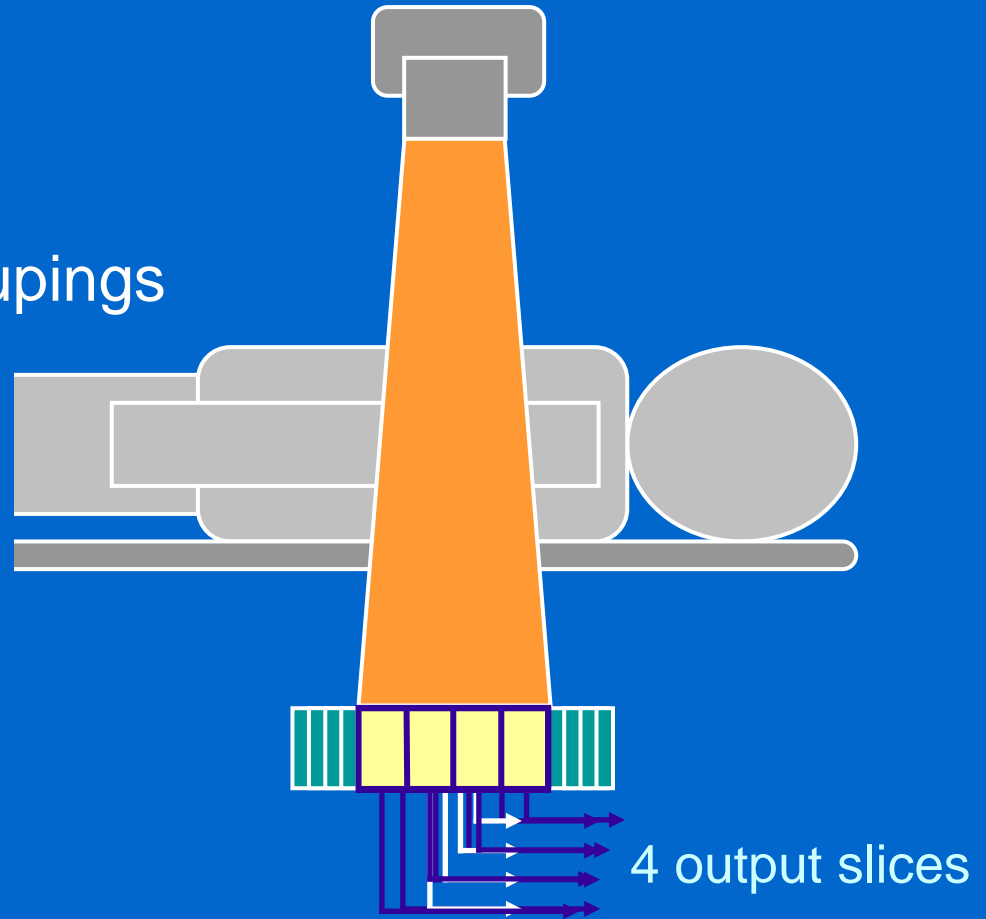
# Slices & detectors

- Just 4 detectors reduces options for scanning
- Narrow coverage
  - eg. 5 mm for  $d=1.25$  mm



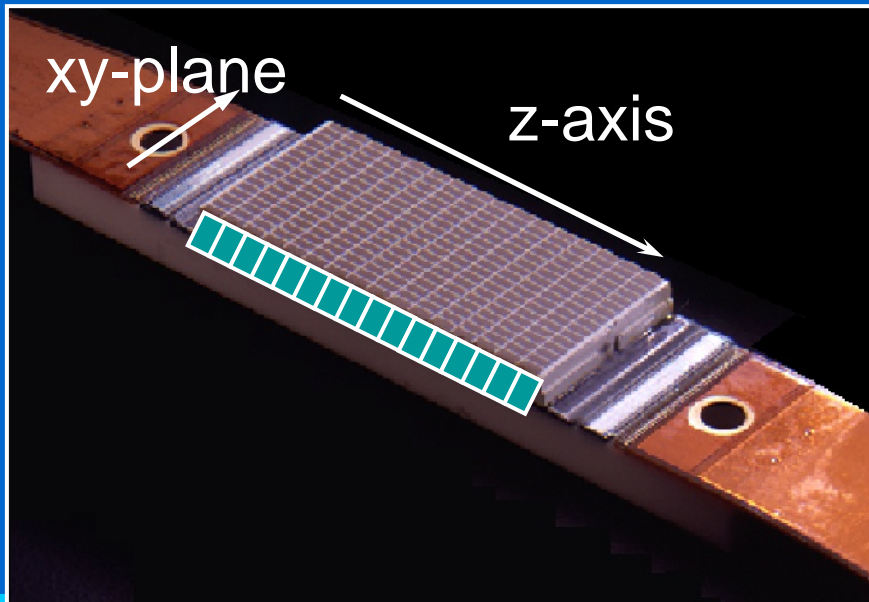
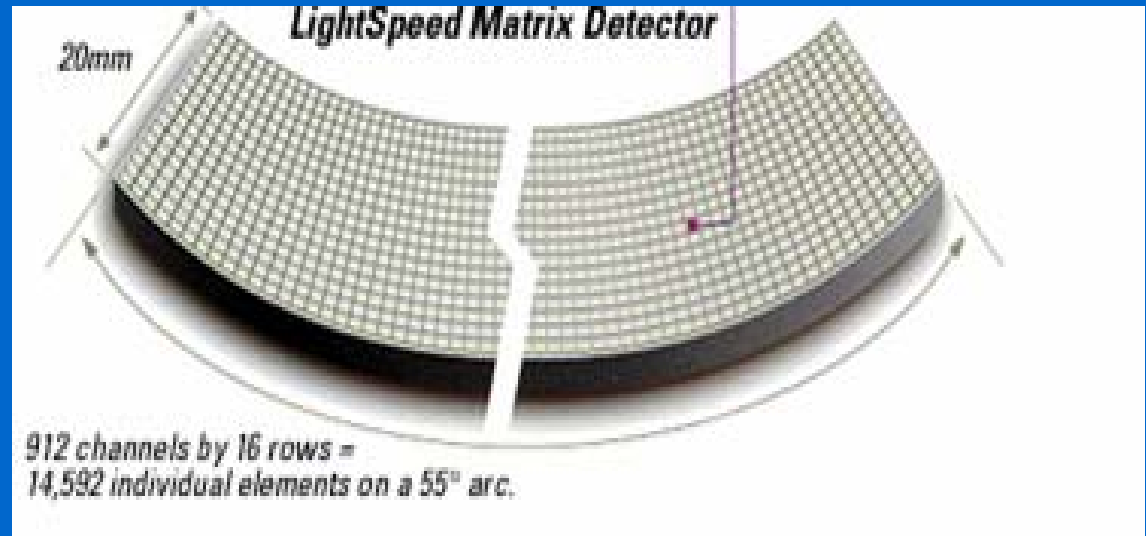
# Slice width selection: 4 slice

- For more flexibility  
AND  
greater coverage  
need more detectors
- Can collect data from groupings of detectors
  - individual detectors
    - $4 \times d$
  - pairs
    - $4 \times 2d$
  - triples
    - $4 \times 3d$



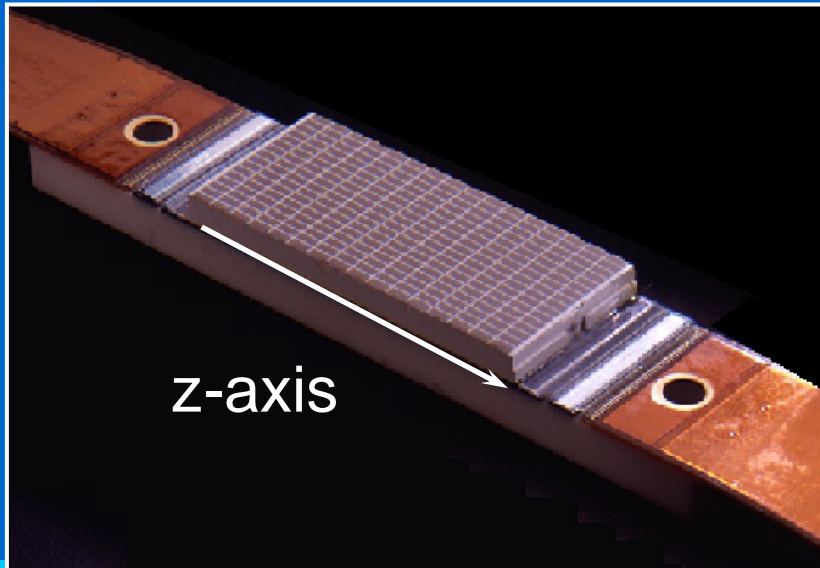
# Slice options: real example

- GE LightSpeed
  - 4 slices
  - 16 detectors in z-axis



# Slice options: real example

- GE LightSpeed
  - 4 slices
  - 16 detectors
- Detector output combined to define data acquisition width
- Coverage up to 20 mm



2 x 0.63 mm



4 x 1.25 mm



4 x 2.5 mm



4 x 3.75 mm

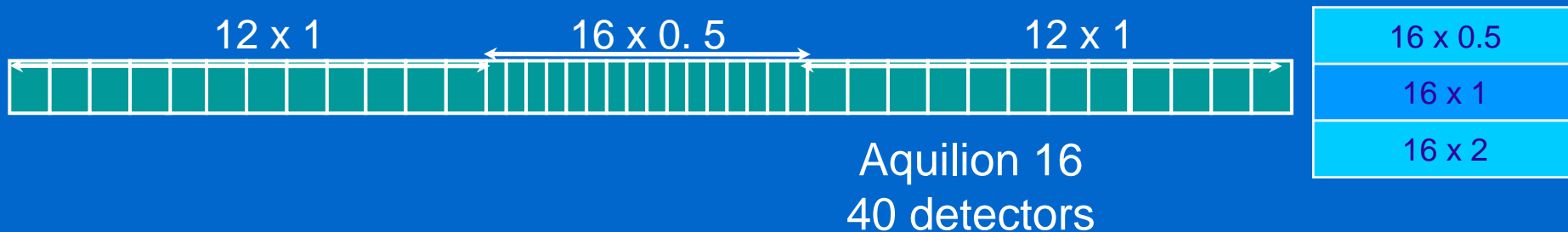
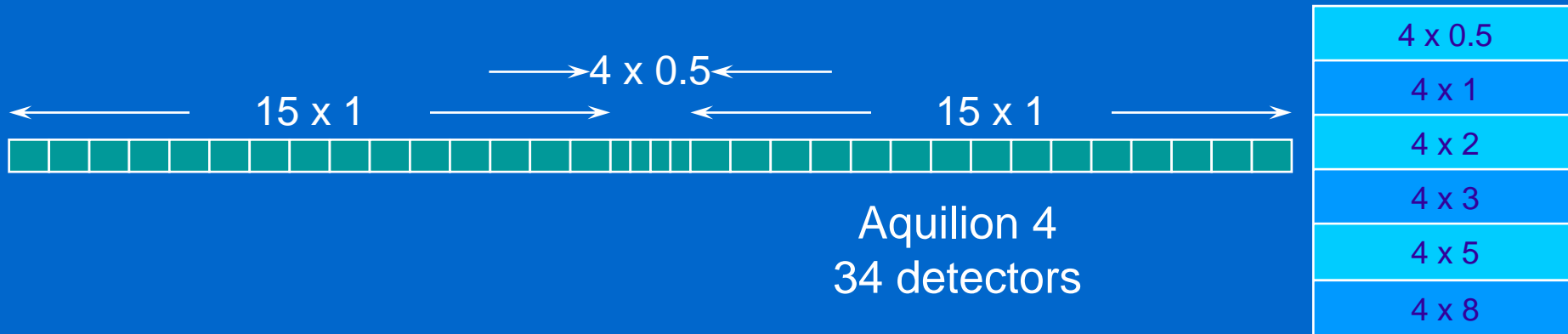


4 x 5 mm

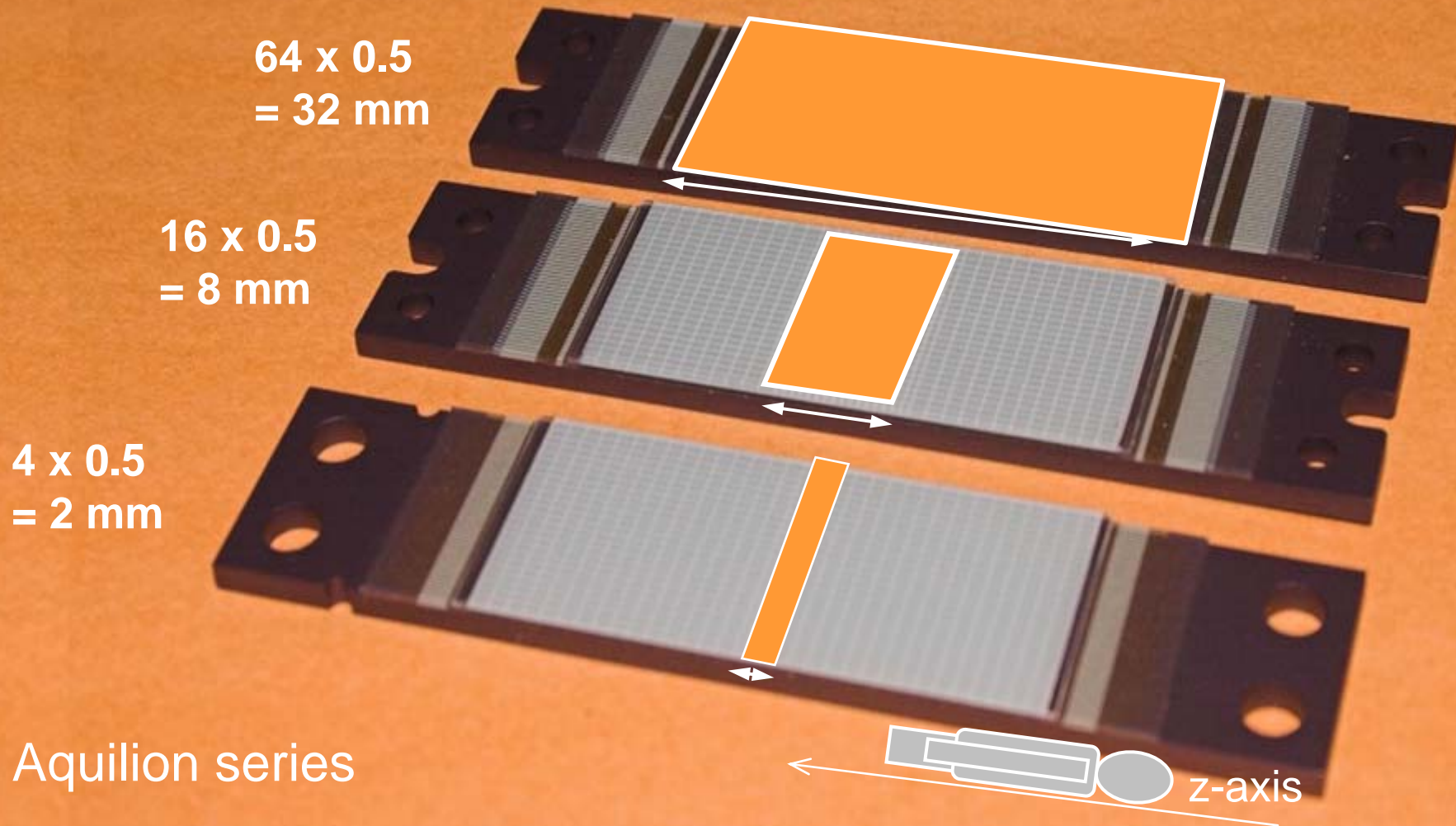


# Adaptive arrays

- Detector elements not all same size
  - e.g. Toshiba Aquillion series



# More “thinnest-slice” coverage



# 64 slice scanners



← 64 x 0.5 →

Toshiba Aquilion 64



← 64 x 0.625 mm →

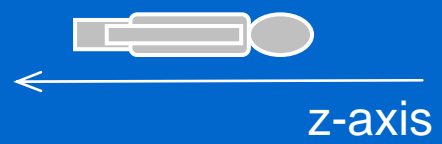
GE LightSpeed VCT

Philips Brilliance CT64



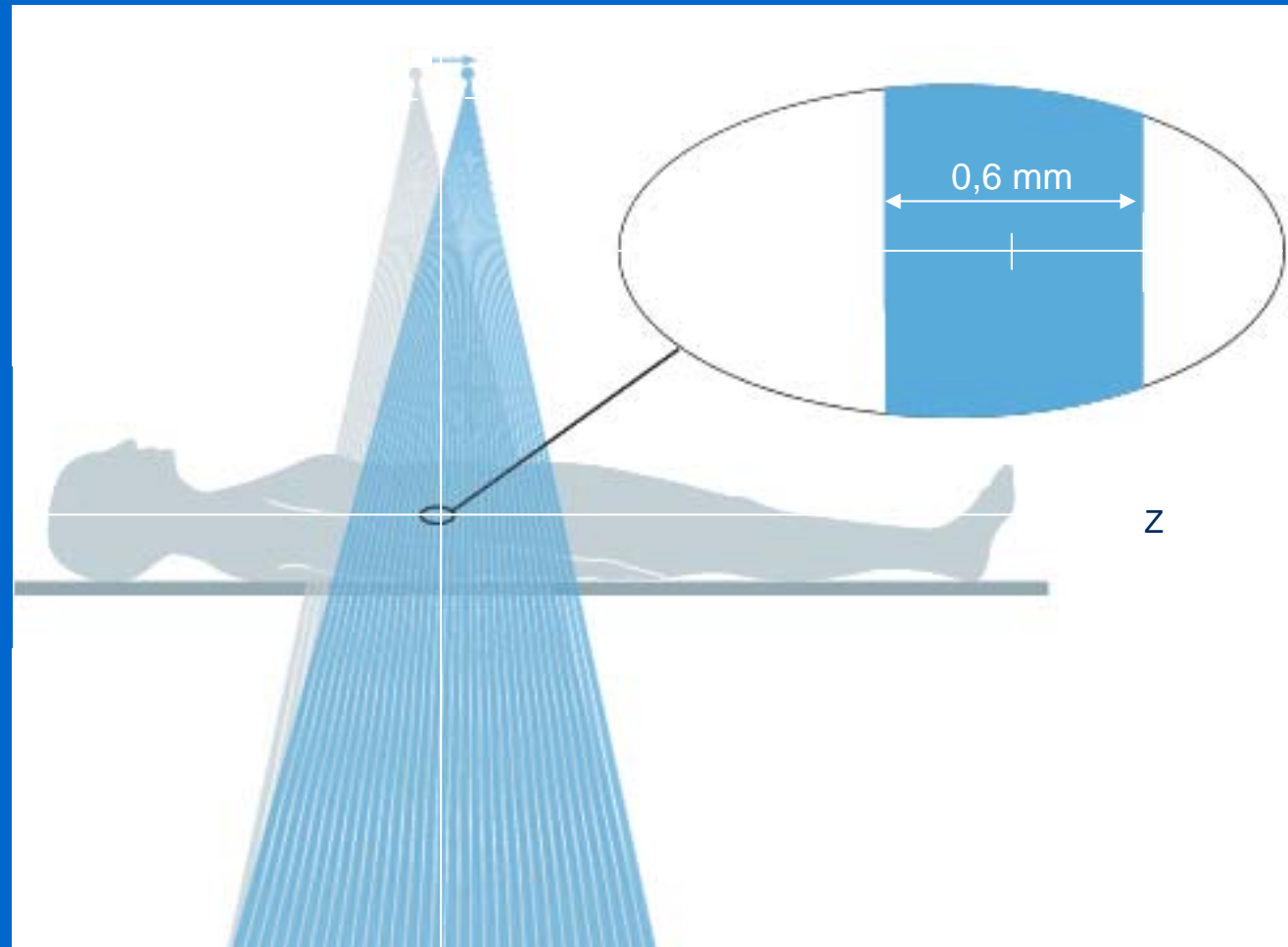
← 4 x 1.2 → ← 32 x 0.6 → ← 4 x 1.2 →

Siemens Sensation 64



# 64-Slice CT: double sampling

- z-flying focal spot
- 32 detectors -> 64 data channels



32 Slice Detection

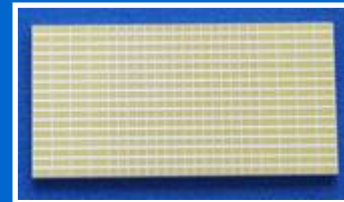
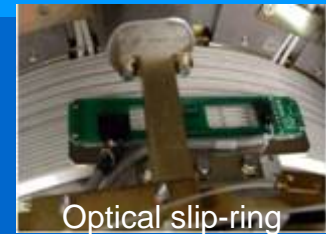
Courtesy Th. Flohr

# ? CT

- Multi-slice CT                      MSCT
  - Multi-detector CT                  MDCT
  - Multi-channel CT                  MCCT
  - Multi-row CT                      (MRCT less common as abbreviation)
- 
- All effectively the same thing
  - Note: care when using “SSCT”
    - normally used for single slice
    - can sometimes refer to single source
      - check the context

# Design considerations

- Scan gantry
  - mechanical stresses
  - data & power feed
- Tubes
  - high currents
    - narrow slices; fast rotations
  - tube cooling
  - generator response
- Detectors
  - responsive
  - efficient
  - small
- Electronics / computers / reconstruction hardware

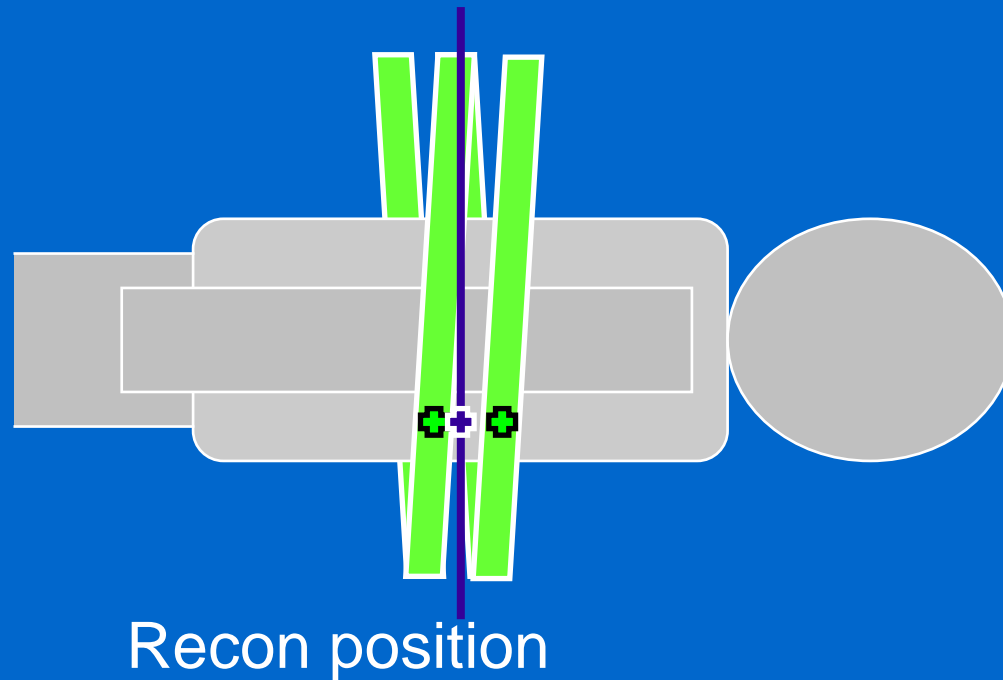


# More challenges for MSCT

- Reconstruction
- Artefacts
- Dose efficiency
- Data management

# Using helical data

- Single slice: interpolate using 2 nearest data points

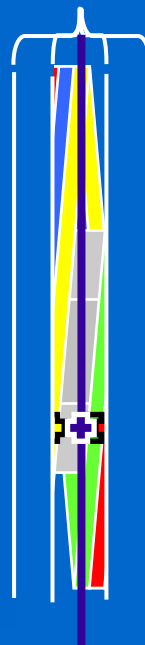




# Using helical data

- Single slice: interpolate using 2 nearest data points
- Up to 8 slice MSCT: use all data within a variable 'filter width' for interpolation

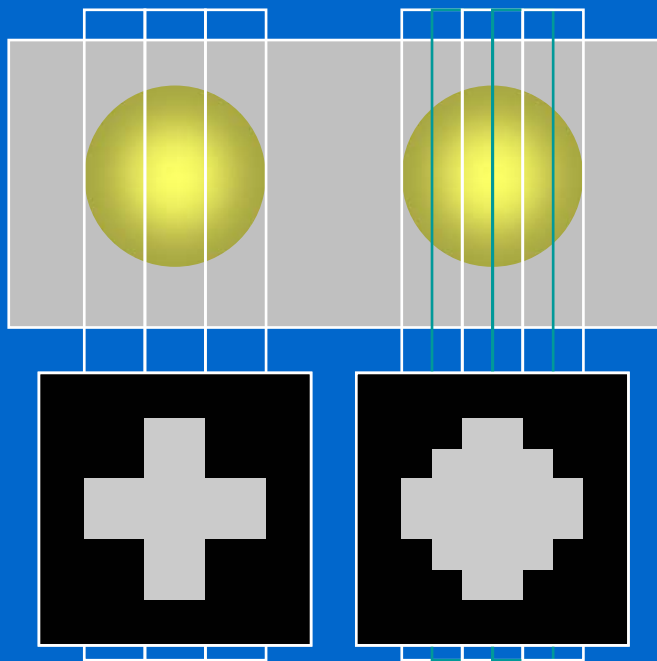
Filter width



Recon position

# Flexibility of reconstruction

- 'Overlapping' reconstructions
  - better z-axis resolution
  - better 3D imaging

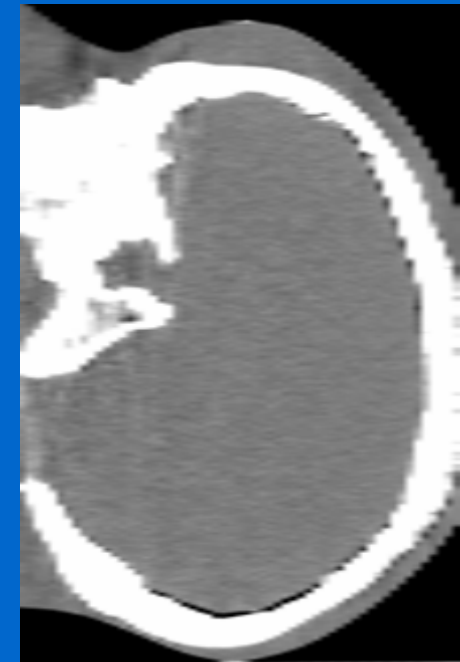


contiguous

Helical,  
overlapping



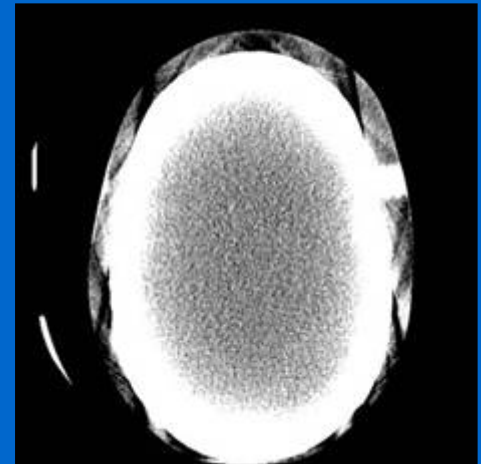
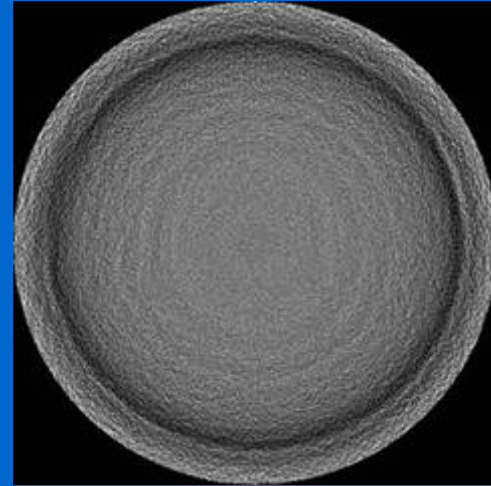
MPR of skull  
from 5mm slices



MPR of skull  
from 5mm slices  
recon every 2.5 mm

# Artefacts

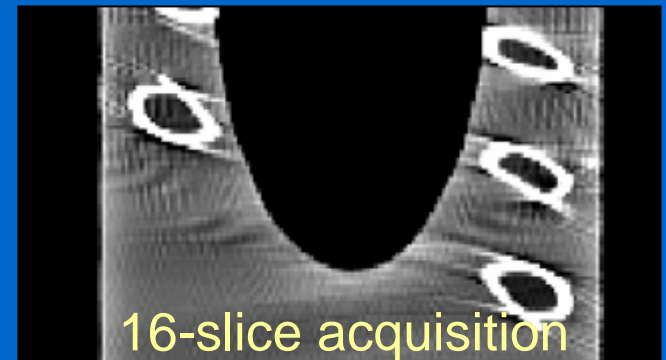
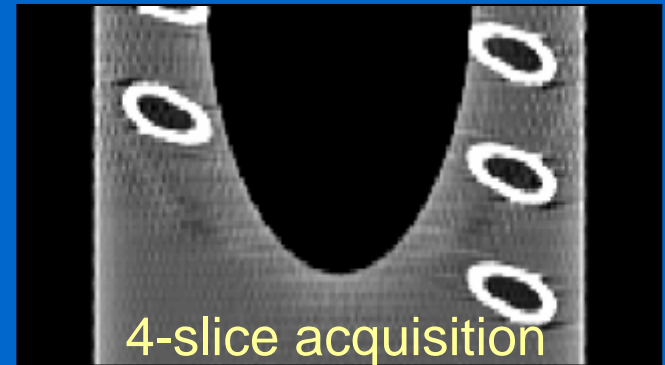
- All standard (SS) CT artefacts can still occur
  - ring artefact
  - beam hardening
- Specific issues for MSCT
  - cone beam
  - helical artefacts



# Cone beam artefacts

- Seen as streaks in image as number of slices increases
- Due to large cone angles and narrow slices

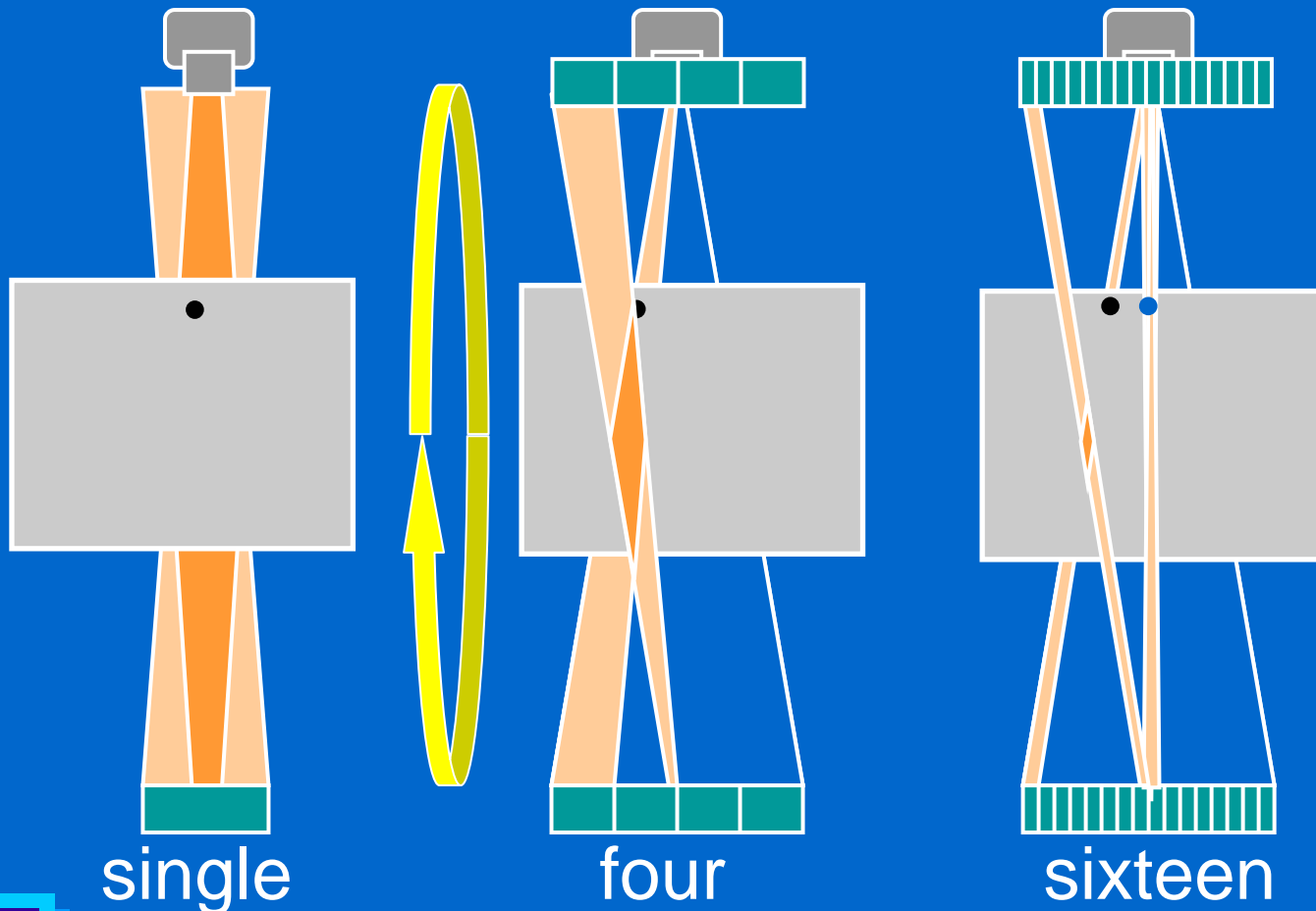
Thorax phantom



Courtesy: Siemens

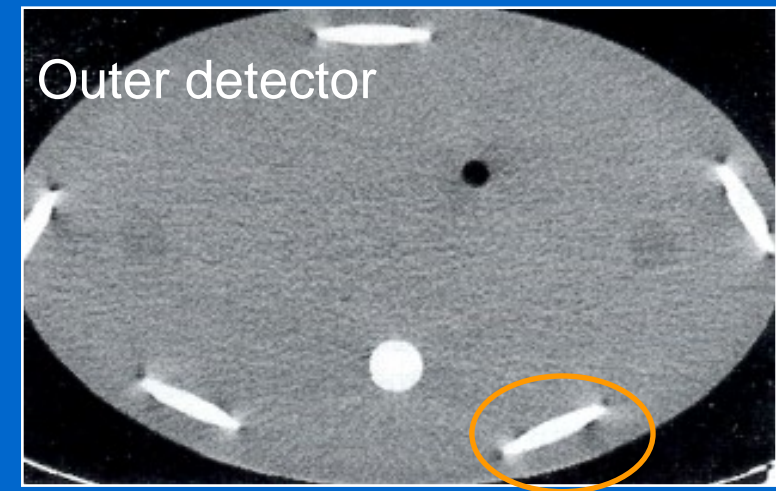
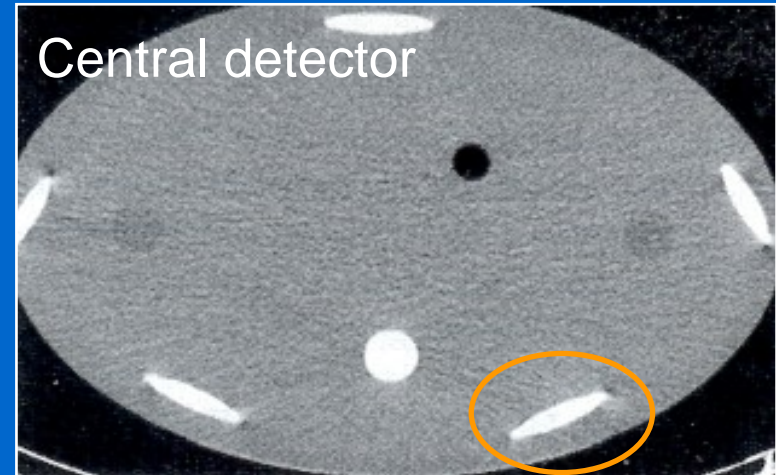
# Cone beam

- As number of slices increases, beam is more diverging, outer slices are distorted
- Negligible up to 8 slices, significant for 16 slice scanners



# Cone beam artefact

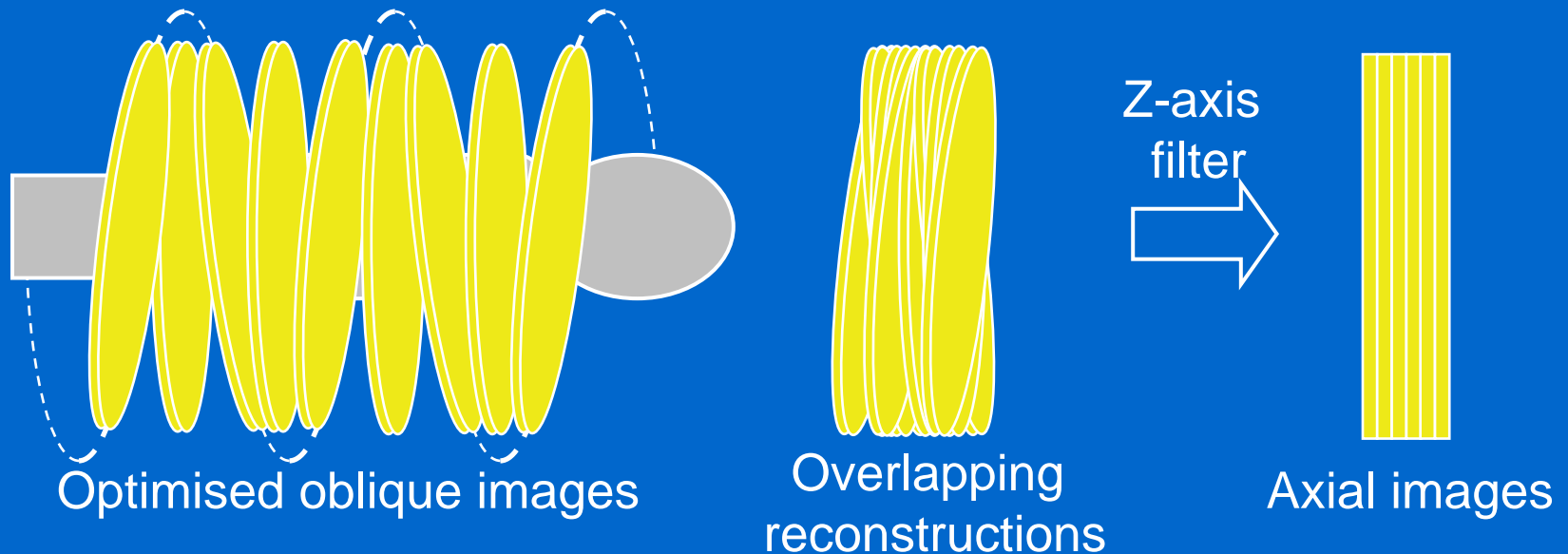
- Beyond 8 slices, special reconstructions needed to avoid cone beam artefacts
- Range of techniques are used
  - tilted (hyperplane, or non-orthogonal)
  - 3D (Feldkamp / FDK) reconstructions



courtesy GE

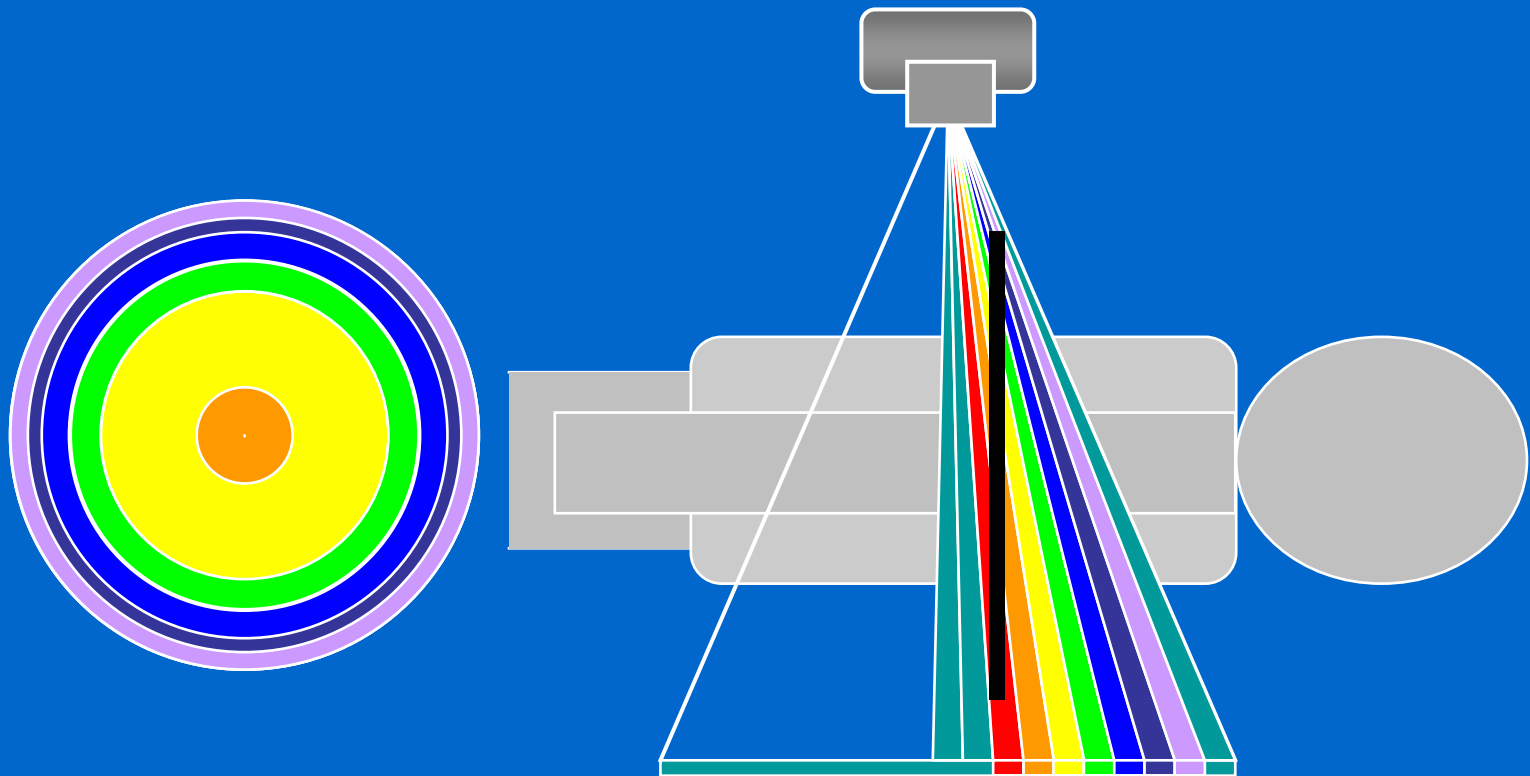
# Tilted reconstruction

- ASSR techniques uses tilted reconstructions
  - images back projected along optimal oblique planes
  - reconstructed images then filtered to produce axial images



# 3D reconstruction

- Feldkamp based three dimensional reconstructions
  - extension of back projection to third dimension
  - requires more computing power



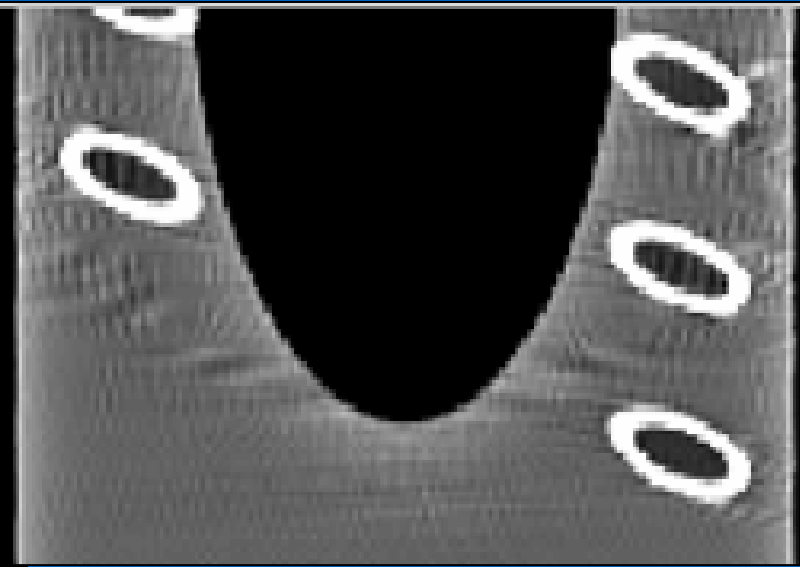


# Effectiveness of cone beam algorithms

## 16-slice acquisition



standard reconstruction

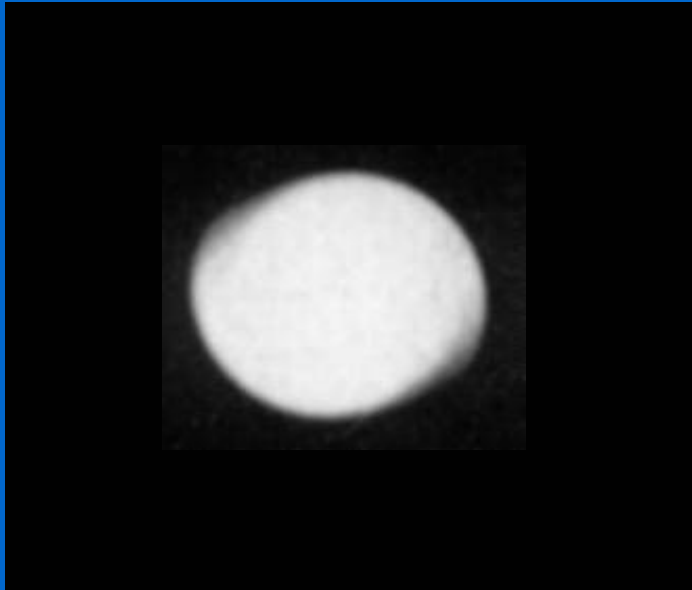


cone beam reconstruction

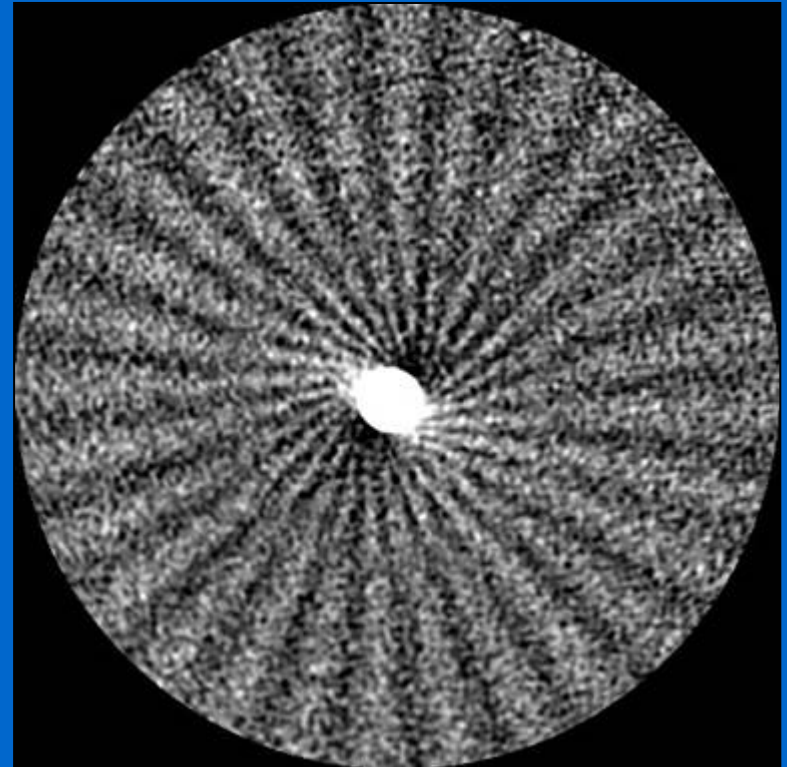
Courtesy: Siemens

# Helical artefacts

- Arise from variation in sampling along the z-axis

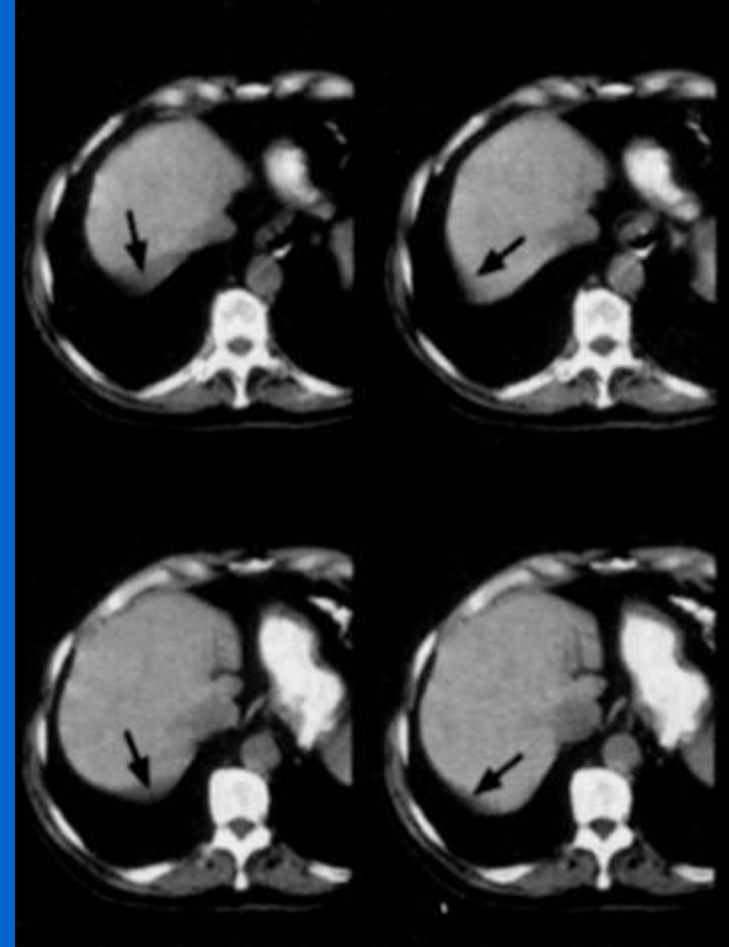
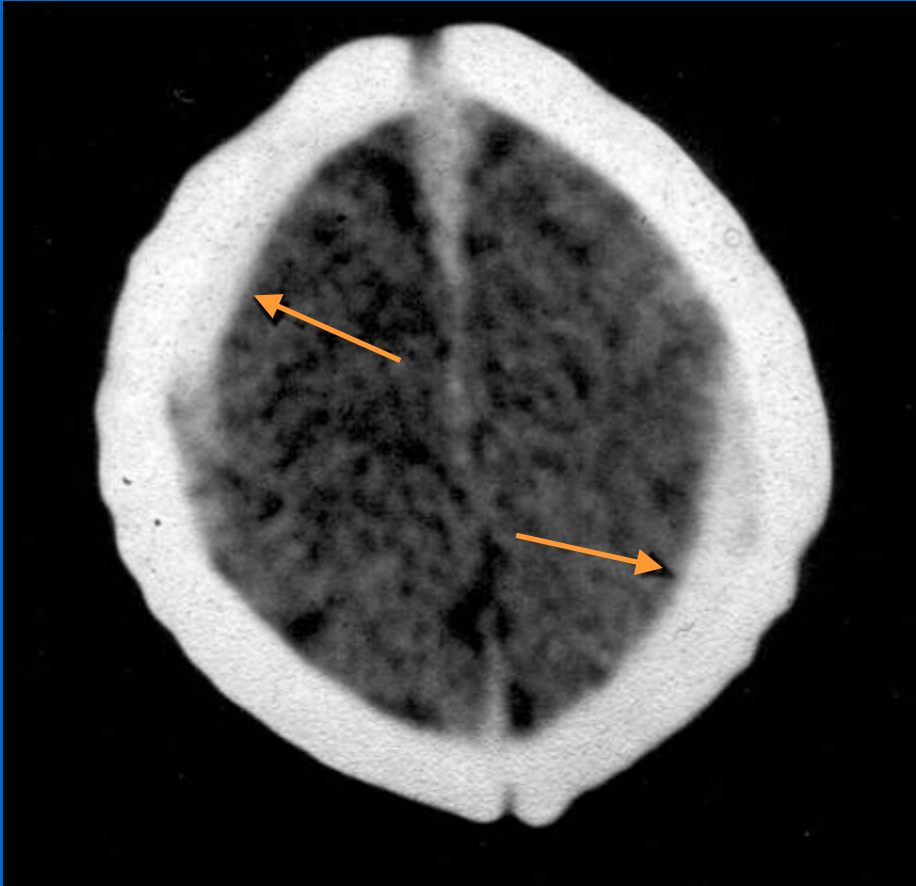


Conical phantom  
single-slice helical



Spherical air pocket  
8 x 2.5 mm slice helical

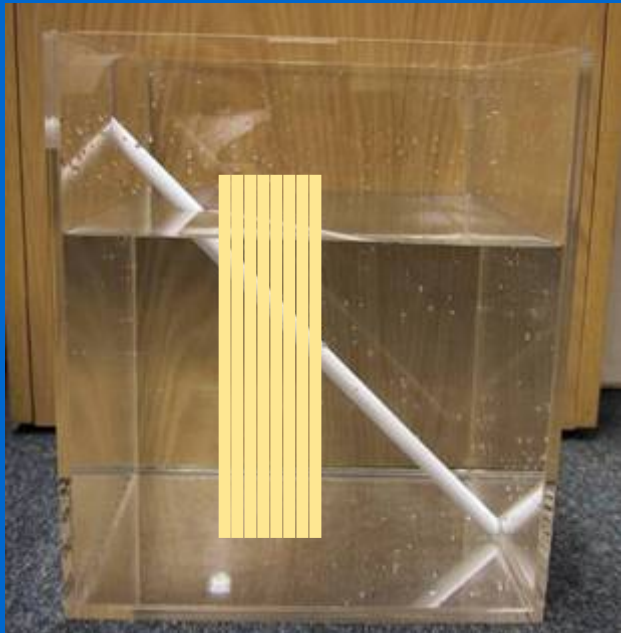
# Helical artefacts - clinically



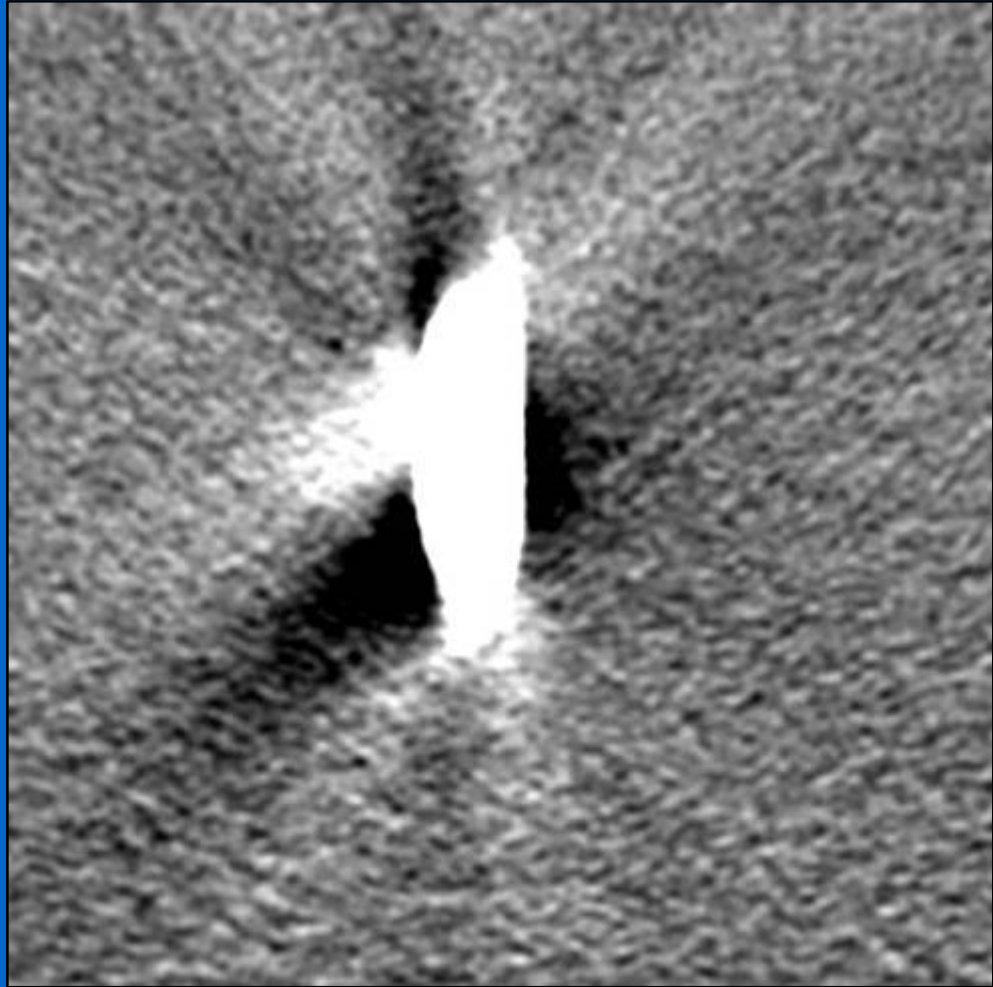
From "Artefacts in spiral-CT images and their relation to pitch and subject morphology", Wilting, JE and Timmer, J. EJR 9(2) 1999

# Windmill artefact in consecutive slices

- Teflon rod at 60° to horizontal

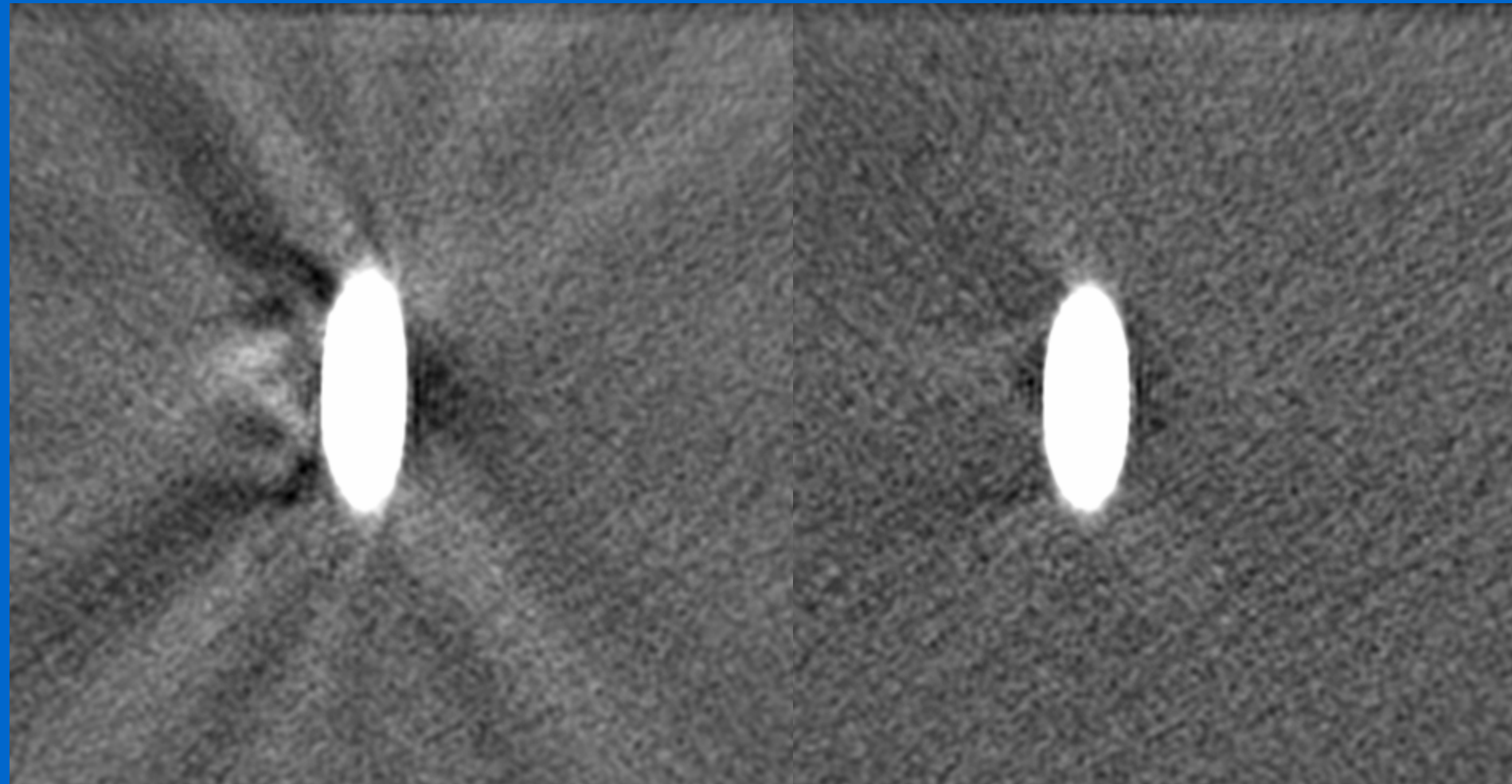


Pitch<sub>x</sub> = 1.5  
16 x 1.5 mm acquisition  
5 mm recon.



# Helical artefact

- Processing can compensate for helical scanning
- Reduces artefact



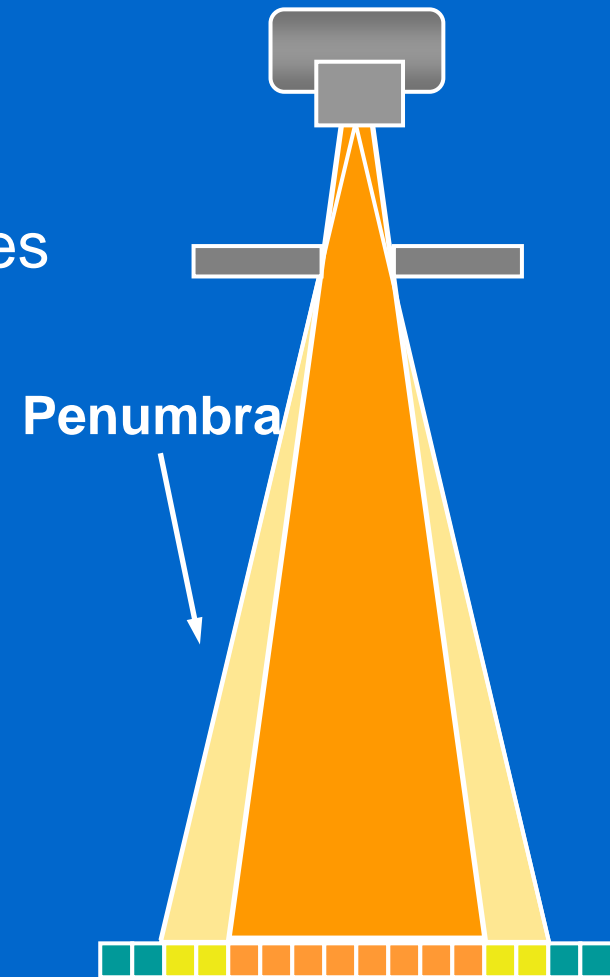
# MSCT and dose

- CT is a high-dose exam
  - more CT studies being undertaken
  - even more exams with new MSCT apps
- Automatic exposure controls (AEC)
- Differences between single and multi-slice
  - over-beaming
  - over-ranging

# Z-axis over-beaming

- Beams are wider than the nominal value
  - due to finite size of focal spot
- Irradiated beam width ~ 3mm wider
  - e.g. 4 x 2.5 mm slices, 12.5 mm beam
- Less significant as beam width increases
  - wider collimations routinely used

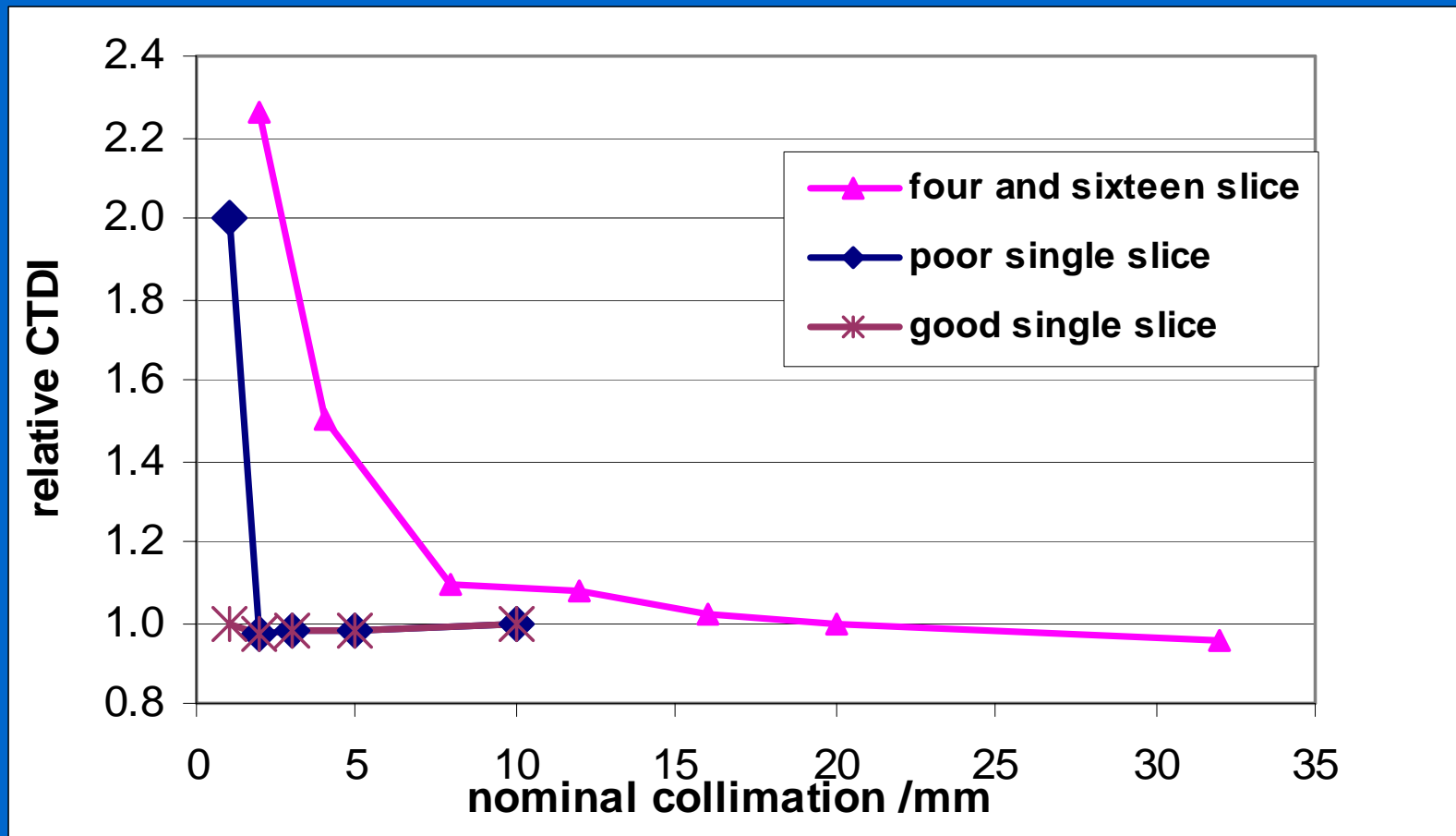
Nominal beam	Excess beam	Geometric Efficiency
10 mm	25%	72%
25 mm	10%	80%
40 mm	6%	95%





# Wider beams – lower dose

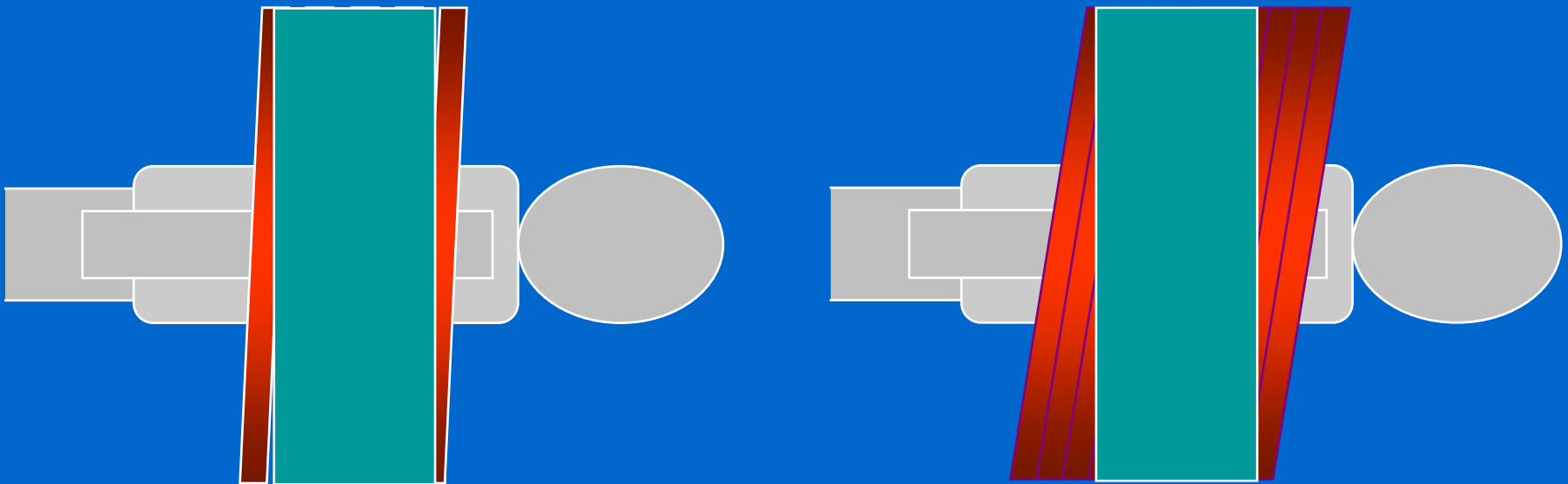
- Efficiency increases with collimation (beam width)
- More coverage means thin slices at lower dose





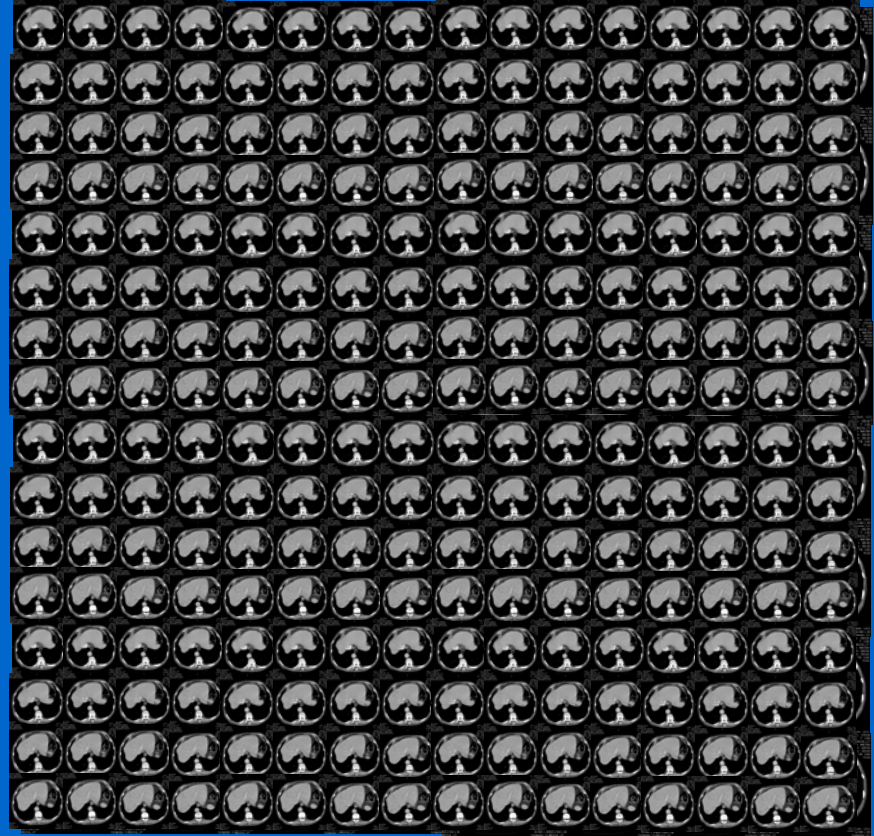
# OVERRANGING

- To image entire volume, data is needed at both ends of scan
  - requires more rotations to acquire
- This is more significant for multi-slice, wider beams, and for short scan ranges



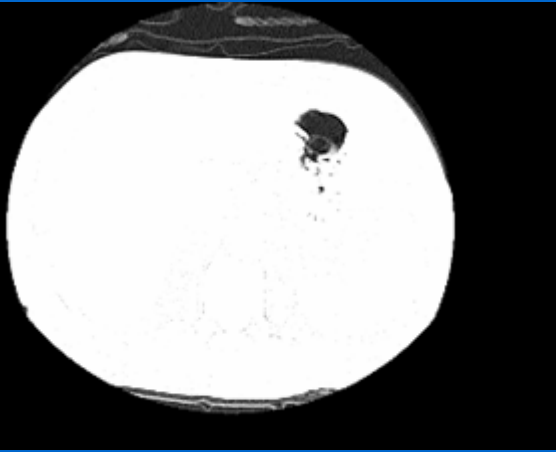
# Data explosion!

- Scan data throughput from gantry to computer
  - Single slice, 1 second rotation : ~ 2 megabytes per second
  - 4 slice, 0.5 s rot : 16 MB/s
  - 16 slice, 0.5 s rot : 64 MB/s
  - 64 slice, 0.5 s rot : 256 MB/s
- Image production speed
  - 2005: ~ 64 MB/s
- Data processing burden
- Network traffic ...
- Archive issues...
- Images per exam
- Image viewing capacity?



# Reporting & navigation tools

- How am I supposed to look at 800 images?



'Stack' View

*"Get in the volume"*



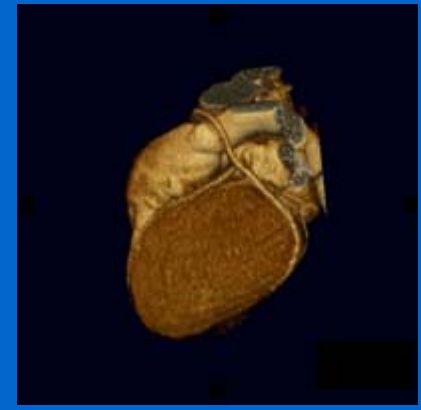
Coronal Slab VR



Axial Slab MIP



MPR



3D VR

# In summary

- Multislice CT scanning has progressed hugely since 1998
  - there are challenges that arise with MSCT – and have been met
    - eg ConeBeam reconstructions
- 16 and 64 slice changes CT from slice to volume scanning
  - image quality can now be routinely isotropic
  - 3D data sets readily available
  - data sets are there to be explored flexibly
- New applications still developing  
... and new scanners coming



# Acknowledgements

- for scanner information & images
  - GE Healthcare
  - Philips Medical
  - Siemens
  - Toshiba
  - University of Erlangen
  - Matthew Benbow, RBCH
- Thanks also due to
  - Sue, Maria and Margaret at ImPACT
  - David Platten & Nick Keat

# Physics & Technology of Multislice CT

[www.impactscan.org](http://www.impactscan.org)

[www.pasa.nhs.uk/cep](http://www.pasa.nhs.uk/cep)