

# Image Quality and Dose Issues in MSCT

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# Image Quality and Dose

- Image quality
  - Image noise
  - Spatial resolution
  - Contrast
  - Artefacts
- Radiation Dose
  - Organ dose
  - Effective dose

'Speckle and sharpness'



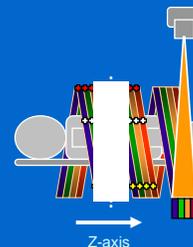
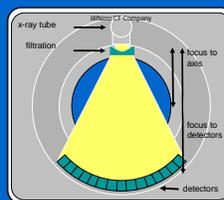
# Image Quality and Dose

- Image quality
  - Image noise
  - Spatial resolution
  - Contrast
  - Artefacts
- Radiation Dose
  - Organ dose
  - Effective dose

*What we find is that they are all in a constant battle with each other – each can only win at the expense of another*

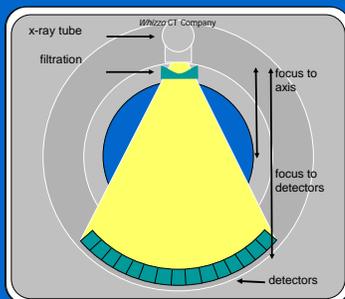
# Image Quality and Dose Issues in MSCT

- Many issues are the same in ss and ms
  - General comments
  - Specific comments to msct
    - tend to relate to z-axis features



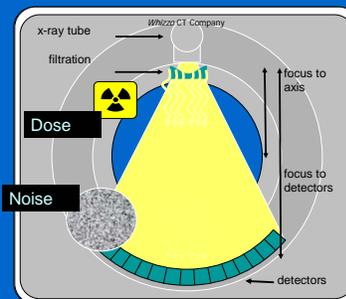
# Scanner parameters affecting IQ and Dose

- Beam shaping filter
- mA
- Scan time
- kV
- Convolution kernel
- Detector size
- No of samples
- Image width
- Beam width
- Pitch



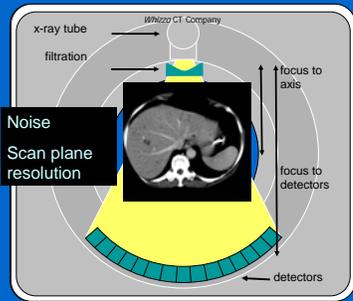
# Scanner parameters affecting IQ and Dose

- Beam shaping filter
- mA
- Scan time
- kV
- Convolution kernel
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- Image width
- Beam width
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## Scanner parameters affecting IQ and Dose

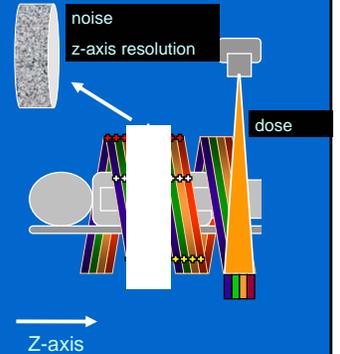
- Beam shaping filter
- mA
- Scan time
- kV
- Convolution kernel
- Detector size
- No. of samples
- Image width
- Beam width
- Pitch



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## Scanner parameters affecting IQ and Dose

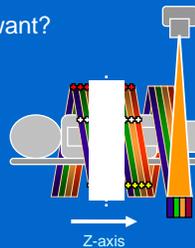
- Beam shaping filter
- mA
- Scan time
- kV
- Convolution kernel
- Detector size
- No. of samples
- Image width
- Beam width
- Pitch



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## IQ and Dose in MSCT

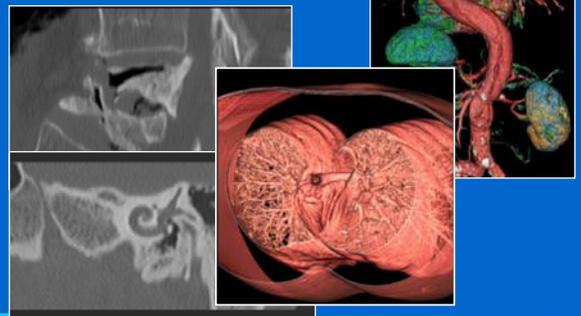
- Spatial resolution (z-axis)
- Pitch
- Dose issues
- Reconstruction algorithm
- What image quality do we want?



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## High contrast spatial resolution

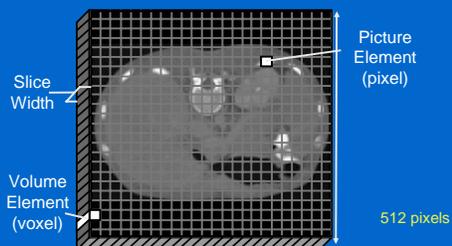
- How small can we go?



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## Spatial Resolution – 3D

- Scan plane (limited by pixel size)
- Z-axis (image slice width)



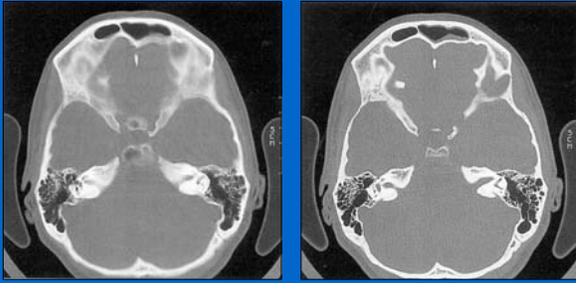
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## Z-axis spatial resolution

- Imaged slice width
  - Influences partial volume artefacts
  - Affects contrast and noise
- In MSCT
  - Flexibility of reconstructing different slice widths
- In helical generally (SS and MS)
  - Optimised by reconstructing overlapping slices

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## Z-axis spatial resolution



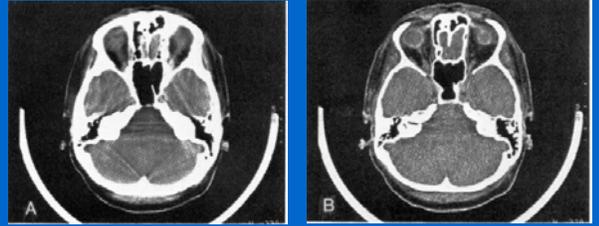
Wider

Narrower

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## Z-axis spatial resolution

- Thinner slice minimises partial volume artefacts



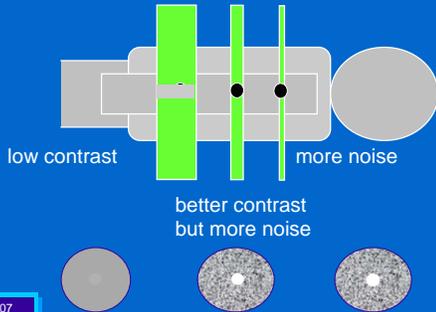
Thick slice

Thin slice

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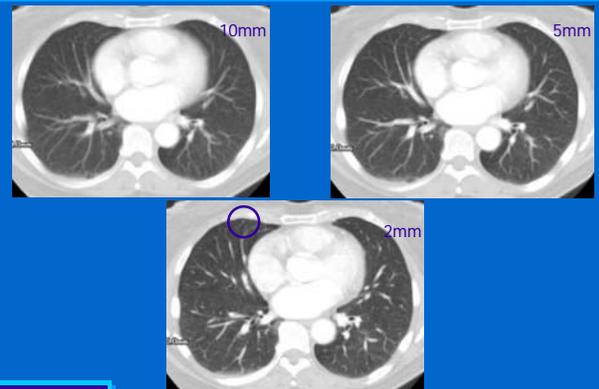
## Z-axis spatial resolution

- Image width affects contrast and noise of object
- Optimised slice width: imaged slice  $\approx$  object size



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## Thinner slice – improved contrast

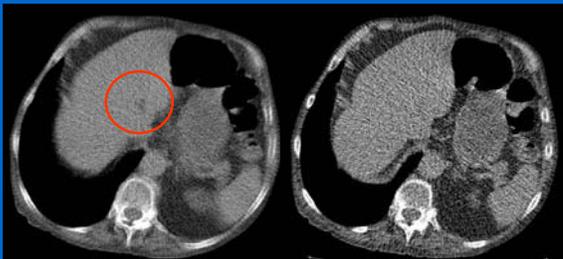


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Courtesy: Matthew Benbow, RBH

## Thinner slice - higher noise

- Object  $\sim$  5 mm



5mm

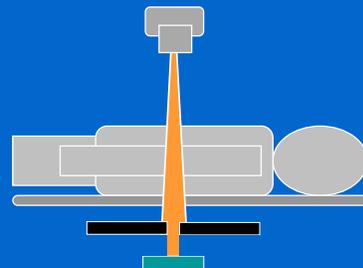
1mm

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Courtesy: Matthew Benbow, RBH

## Z-axis resolution in single-slice

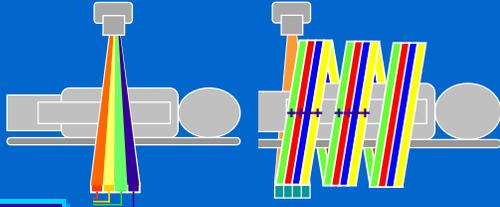
- Image width depended on beam width  
– And post patient collimation for thin slices



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## Z-axis resolution in multi-slice

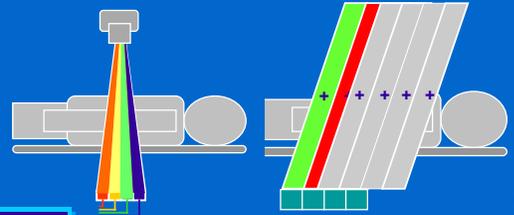
- Image width depends on detector acquisition width
  - eg 4 x 5mm, will not give a 2.5 mm slice! (Use 8 x 2.5)
- May be optimised in helical
  - with closer z-axis sampling (eg z-sharp in Siemens, or certain overlapping pitches)



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## Z-axis resolution in multi-slice

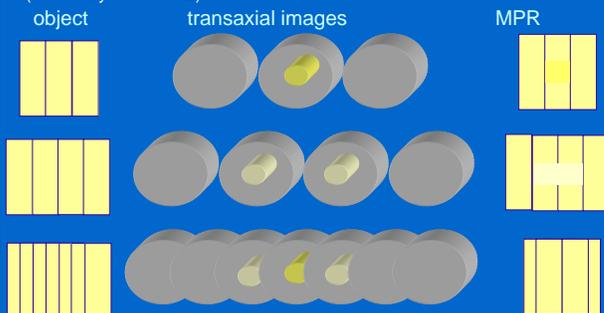
- Image width depends on detector acquisition width
  - eg 4 x 5mm, will not give a 2.5 mm slice! (Use 8 x 2.5)
- May be optimised in helical
  - with closer z-axis sampling (eg z-sharp in Siemens, or certain overlapping pitches)



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## Optimising z-axis spatial resolution

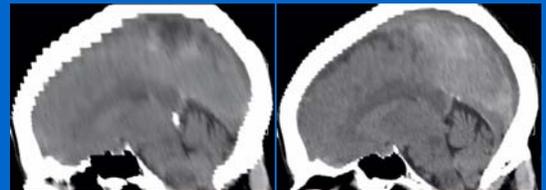
- Visualisation optimised by overlapping reconstructions (viewed by cine or 3-D)



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## Optimising z-axis spatial resolution

- Overlapping reconstructions recommended for optimum contrast and z-axis resolution
- 1/2 to 2/3rds overlap recommended



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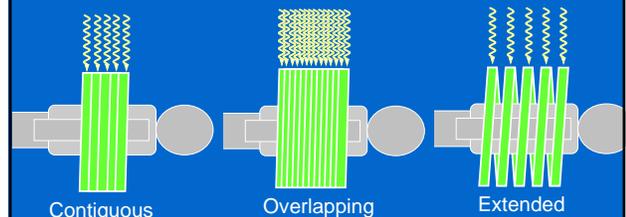
## Effect of pitch

- SSCT vs MSCT
  - Dose
  - Noise
  - Image slice thickness
- Artefacts

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## Pitch – dose

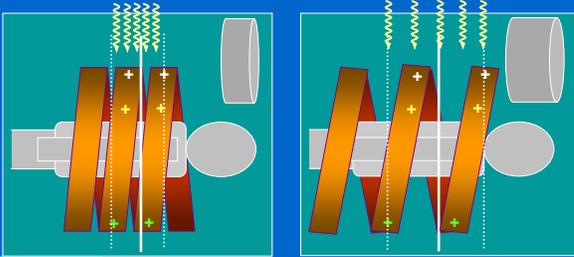
- Overlapping pitch – average dose increases
- Extended pitch – average dose lower



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## Pitch - single slice (increase pitch, mA const)

- Dose decreases
- Noise constant with pitch
  - Two point interpolation regardless of spacing
- Image width increases

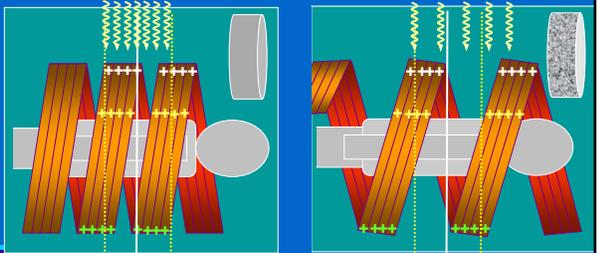


2-point interpolation (360L shown)

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## Pitch – multislice (inc. pitch, mA const.)

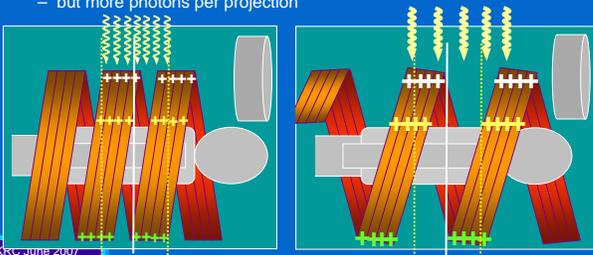
- Dose decreases
- Same filter width
  - Image width remains the same
- Noise increases:
  - less projection data within filter width



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## Pitch – multislice (inc. pitch, inc. mA)

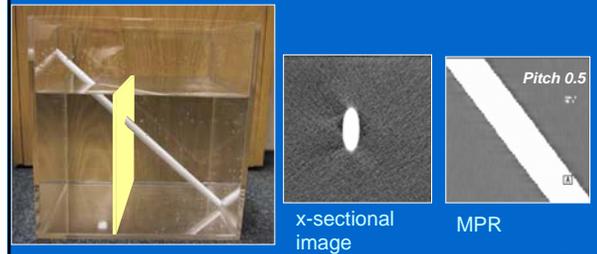
- Dose stays the same
- Same filter width
  - Image width remains the same
- Noise stays the same:
  - less projection data within filter width,
  - but more photons per projection



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## Pitch – artefacts

- Teflon (PTFE) rod in water
  - to simulate rib at an angle to scan plane
- Spiral Artefacts in MPRs

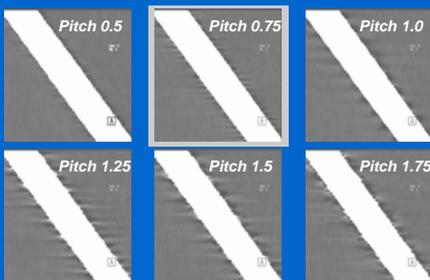


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## Pitch – artefacts

- Spiral Artefacts in MPRs of a Tilted Teflon Rod
  - image-width 3mm
  - acquired using 4\*2.5mm (Siemens Volume Zoom)

gradual decrease of image quality

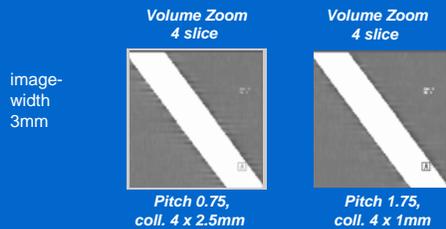


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images courtesy Kalender

## Pitch – artefacts

- Spiral Artefacts in MPRs of a Tilted Teflon Rod



- For a given image width:
  - small detector acquisition width at higher pitch is better than wide acquisition width at lower pitch

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courtesy Kalender

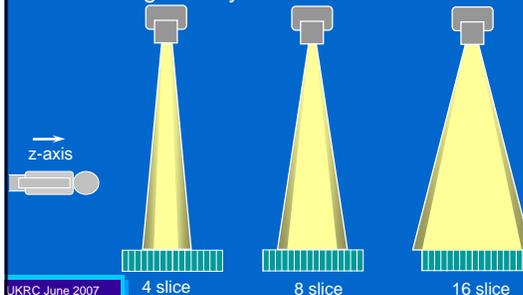
## Dose issues in MSCT

- Beam width (overbeaming)
- Helical overscan (overranging)

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## Dose issues in MSCT - Beam width

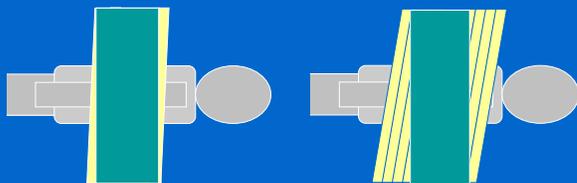
- Penumbra typically 3 mm for all beam widths
  - lower proportion of total dose with wider beam widths
- Wider is generally better



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## Dose issues in MSCT - Overranging

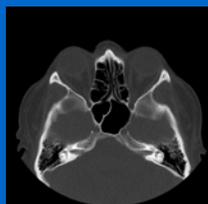
- Except for short scan lengths and large pitches near sensitive organs
  - Use narrower beam widths, or axial scans



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## Effect of reconstruction filter

- Filter used in backprojection (convolution kernel)
  - Smooth, standard, detail, bone
  - AH30, AH40, AB50
  - FC41, FC43 etc, etc
- Used to optimise spatial resolution against noise



Smooth

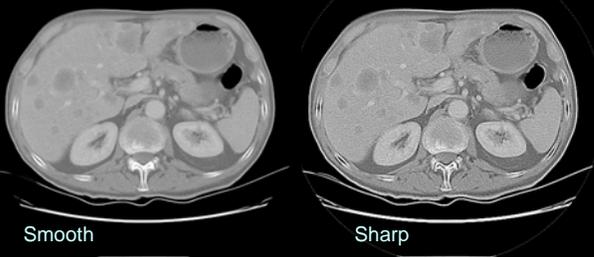


Sharp

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## Effect of reconstruction filter

higher spatial frequency  $\Rightarrow$  more noise



eg Smooth  $\rightarrow$  Standard  $\rightarrow$  Sharp  
noise = ~ 7 HU  $\rightarrow$  17 HU  $\rightarrow$  70 HU

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## Tube current

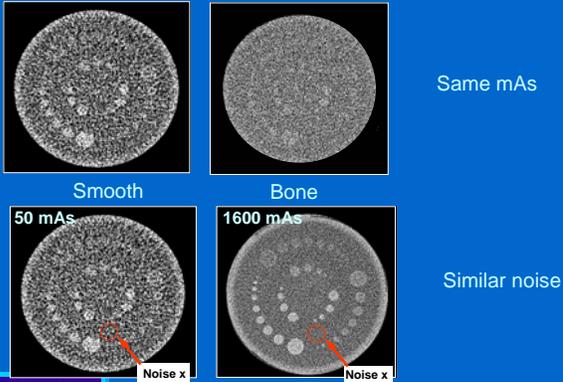


Lower mAs

200 to 100 mAs  $\Rightarrow$  noise x 1.4

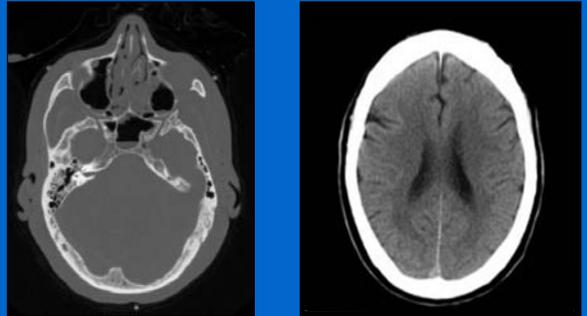
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## Low contrast detectability – recon filter



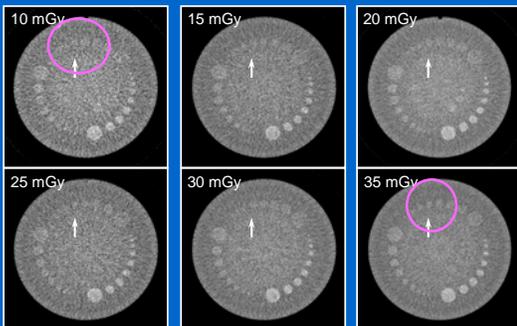
## Compromise depending on requirements

- High spatial detail
- Low contrast resolution



## Image noise

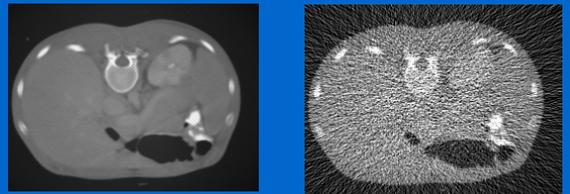
- What is an appropriate level of image noise ?



Doses given are CTDI measured at surface of Catphan

## Image noise

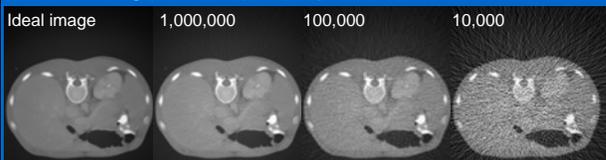
- What is an appropriate level of image noise ?
  - too low – high dose
  - too high – no diagnosis / missed diagnosis
- How do we find the optimum level?



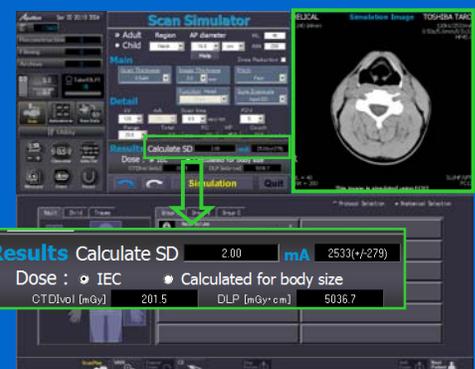
## Systematic addition of image noise

- Systematic addition of noise to clinical images/raw data
  - Simulate mAs
- Studies for a variety of clinical conditions and scanners

decreasing photons per projection →

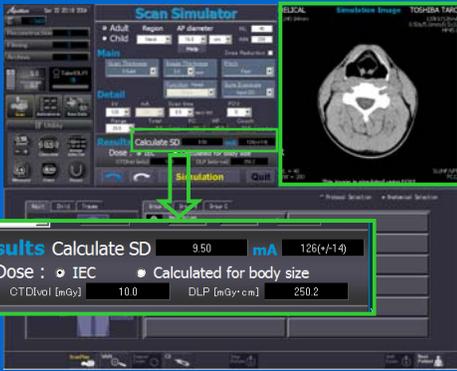


## Image quality required for diagnosis



Scan Simulator: Courtesy of Toshiba

## Image quality required for diagnosis

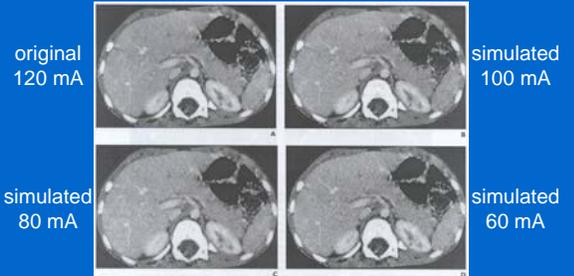


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Scan Simulator: Courtesy of Toshiba

## Systematic addition of image noise

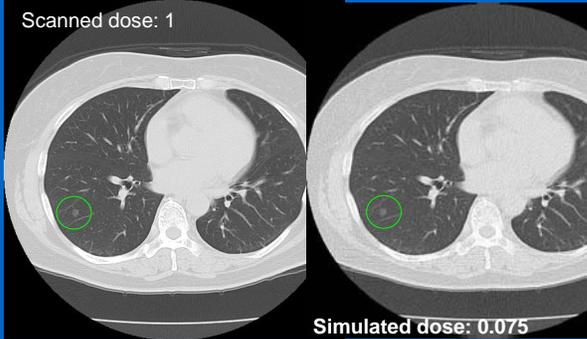
- Frush et al 'Computer simulated radiation dose reduction for abdominal multidetector CT of Pediatric patients' AJR:179, November 2002



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## What noise level is needed?

Scanned dose: 1



Simulated dose: 0.075

Images courtesy Y. Muramatsu, NCC Tokyo

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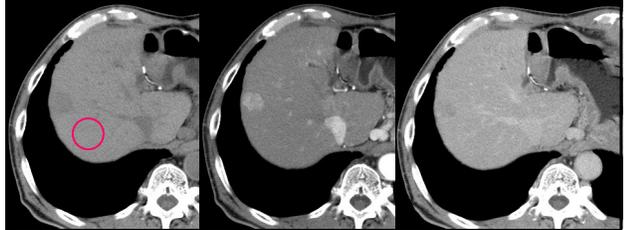
## What noise level is needed?

Original (16 x 1 mm, 200 mAs, pitch 0.9375)

Plain (no contrast)

Early

Late



Scanned dose : 1.0

Noise SD: 8.0

Images courtesy Y. Muramatsu, NCC Tokyo

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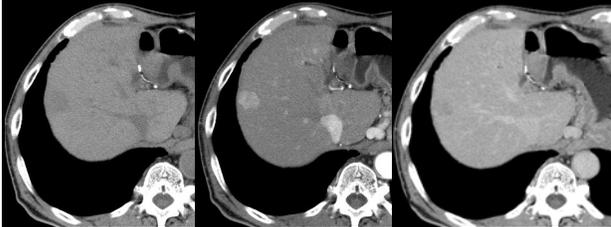
## What noise level is needed?

Simulation

Plain

Early

Late



Dose Ratio: 0.83

SD: 8.5

Images courtesy Y. Muramatsu, NCC Tokyo

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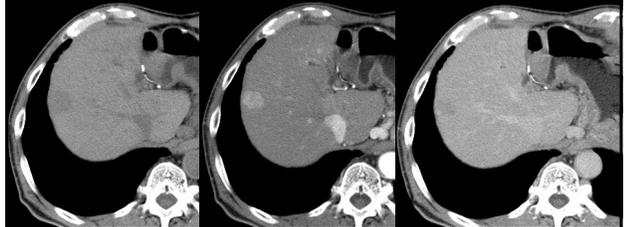
## What noise level is needed?

Simulation

Plain

Early

Late



Dose Ratio: 0.67

SD: 9.0

Images courtesy Y. Muramatsu, NCC Tokyo

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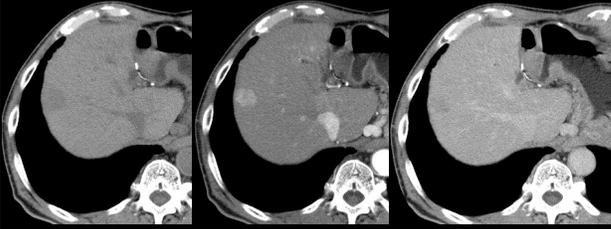
## What noise level is needed?

Simulation

Plain

Early

Late



Dose Ratio: 0.50

SD: 10.0

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Images courtesy Y. Muramatsu, NCC Tokyo

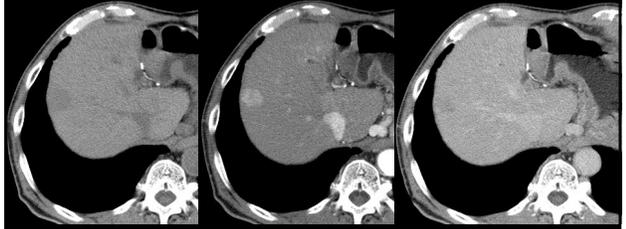
## What noise level is needed?

Simulation

Plain

Early

Late



Dose Ratio: 0.33

SD: 11.5

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Images courtesy Y. Muramatsu, NCC Tokyo

## What noise level is needed?

Simulation

Plain

Early

Late



Dose Ratio: 0.25

SD: 13.5

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Images courtesy Y. Muramatsu, NCC Tokyo

## What noise level is needed?

Simulation

Plain

Early

Late



Dose Ratio: 0.17

SD: 16.5

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Images courtesy Y. Muramatsu, NCC Tokyo

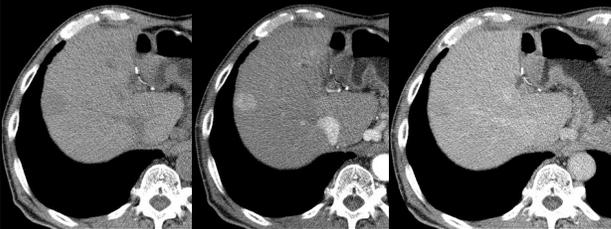
## What noise level is needed?

Simulation

Plain

Early

Late



Dose Ratio: 0.13

SD: 19.5

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Images courtesy Y. Muramatsu, NCC Tokyo

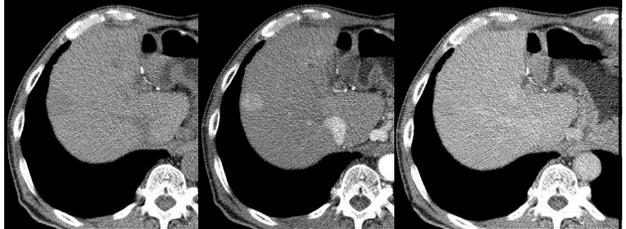
## What noise level is needed?

Simulation

Plain

Early

Late



Dose Ratio: 0.08

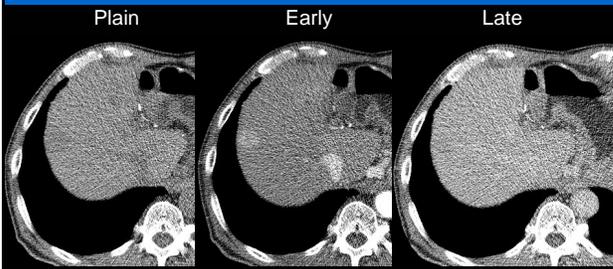
SD: 25.0

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Images courtesy Y. Muramatsu, NCC Tokyo

## What noise level is needed?

Simulation



Dose Ratio: 0.04

SD: 42.0

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Images courtesy Y. Muramatsu, NCC Tokyo

## IQ and Dose in MSCT

- Spatial resolution (z-axis)
- Pitch
- MSCT dose issues
- Reconstruction algorithm
- What image quality do we want?

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## Image Quality and Dose Issues in MSCT

S. Edyvean



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